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(12) United States Patent

Suddaby

(54) STAND-ALONE EXPANDABLE INTERBODY SPINAL FUSION DEVICE WITH LOCKING MECHANISM

(71) Applicant: Loubert S. Suddaby, Orchard Park,

NY (US)

(72) Inventor: Loubert S. Suddaby, Orchard Park,

NY (US)

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(51) Int. Cl.

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 (2006.01)

 A61F 2/30
 (2006.01)

 A61F 2/46
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(52) U.S. Cl.

(58) Field of Classification Search

CPC A61F 2/44; A61F 2/447 See application file for complete search history.

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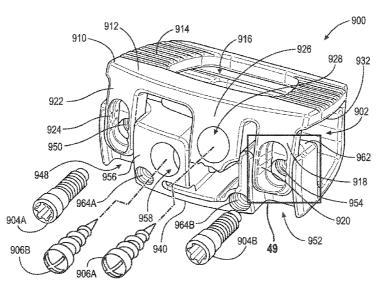
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Primary Examiner — Christopher J Beccia (74) Attorney, Agent, or Firm — Simpson & Simpson, PLLC

(57) ABSTRACT

An expandable interbody spinal fusion device, including an inferior component including at least one hole, a superior component connected to the inferior component, the superior component including a plurality of catches operatively arranged to align with the at least one hole, and a locking screw operatively arranged to engage the plurality of catches and the at least one hole to lock the superior component with respect to the inferior component.

20 Claims, 32 Drawing Sheets



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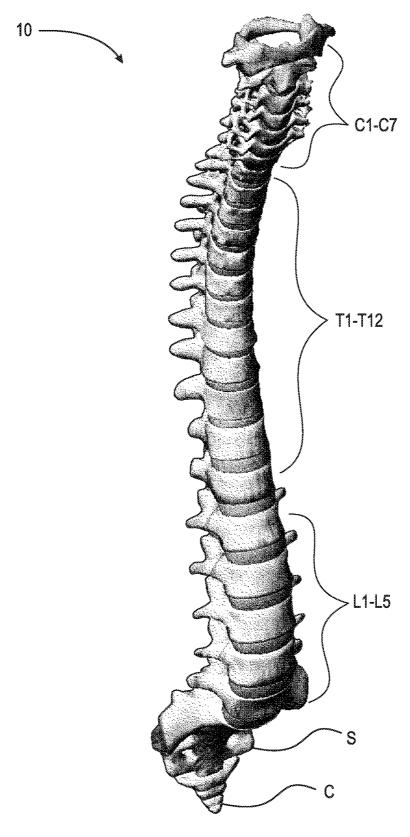


Fig. 1

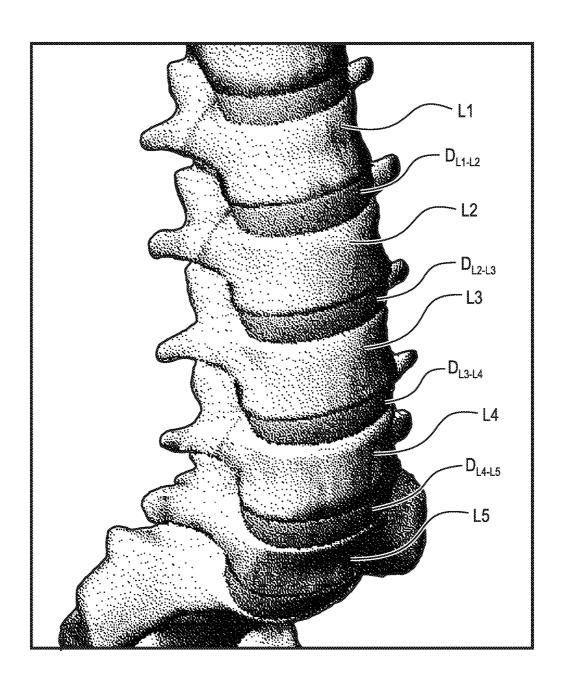
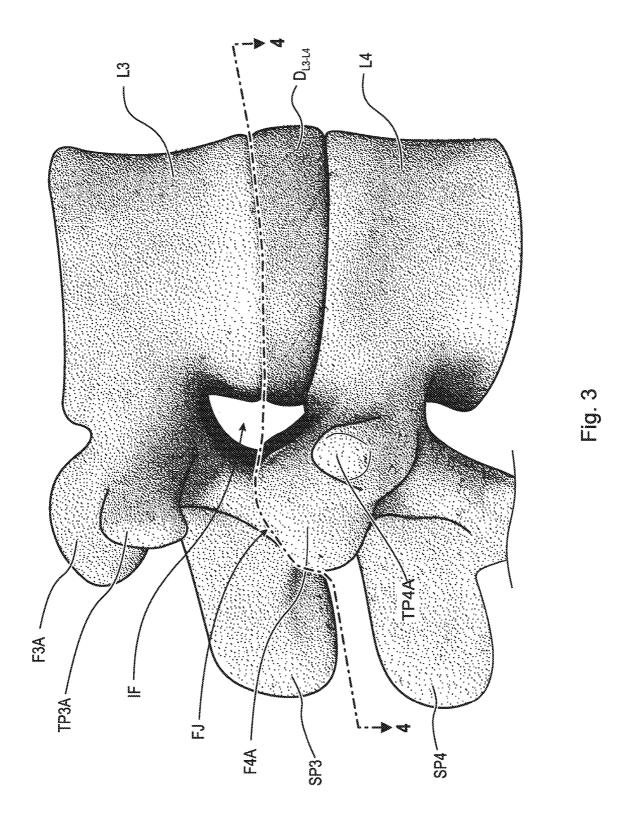


Fig. 2



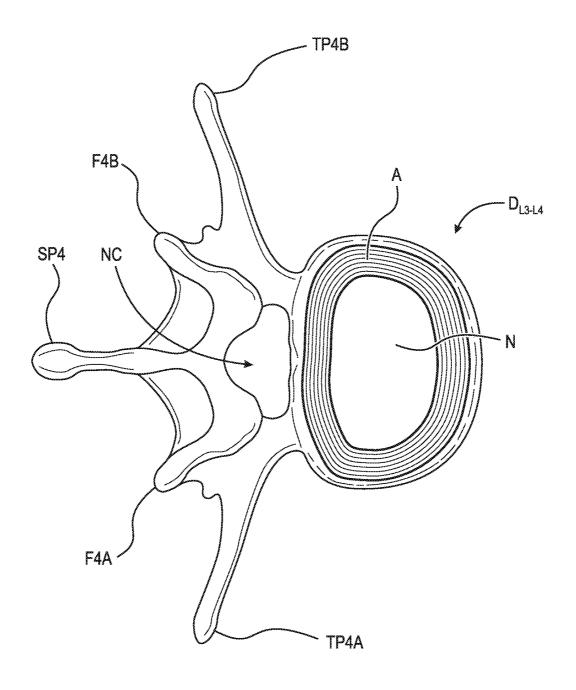


Fig. 4

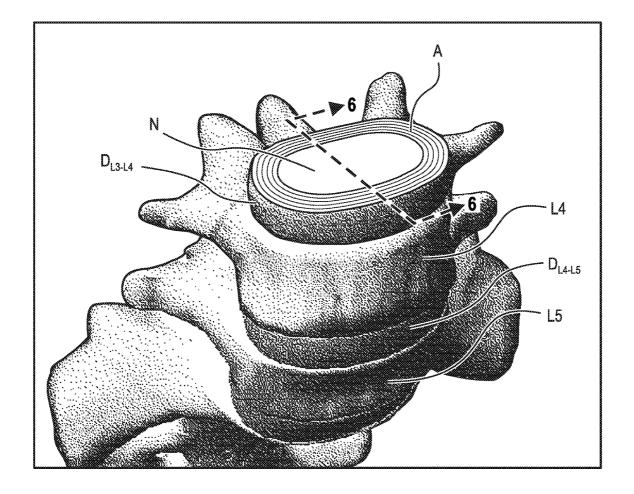
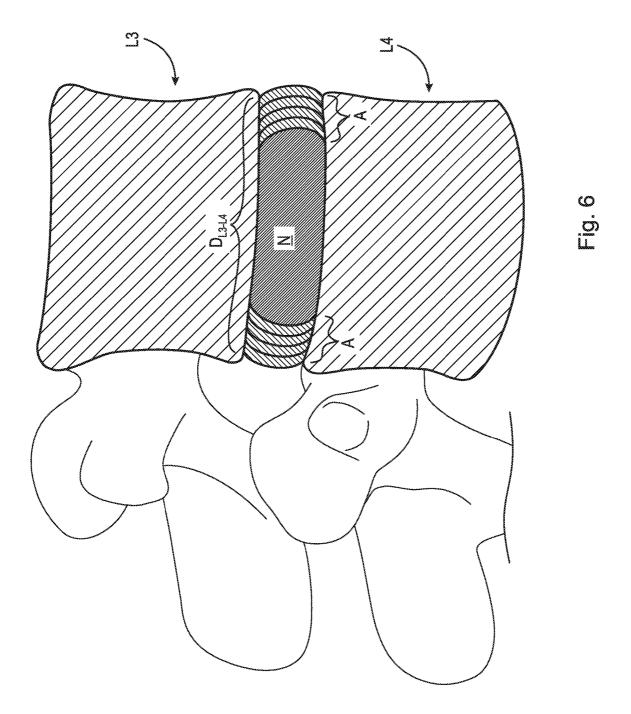
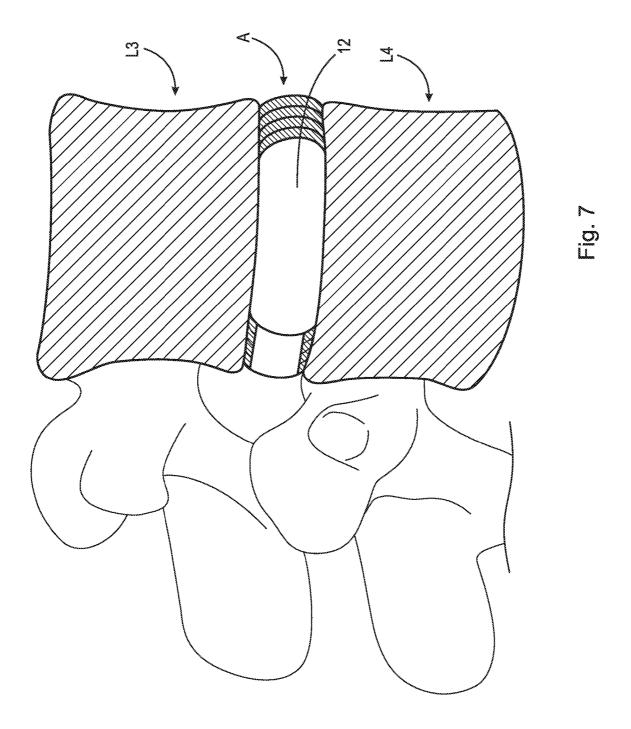
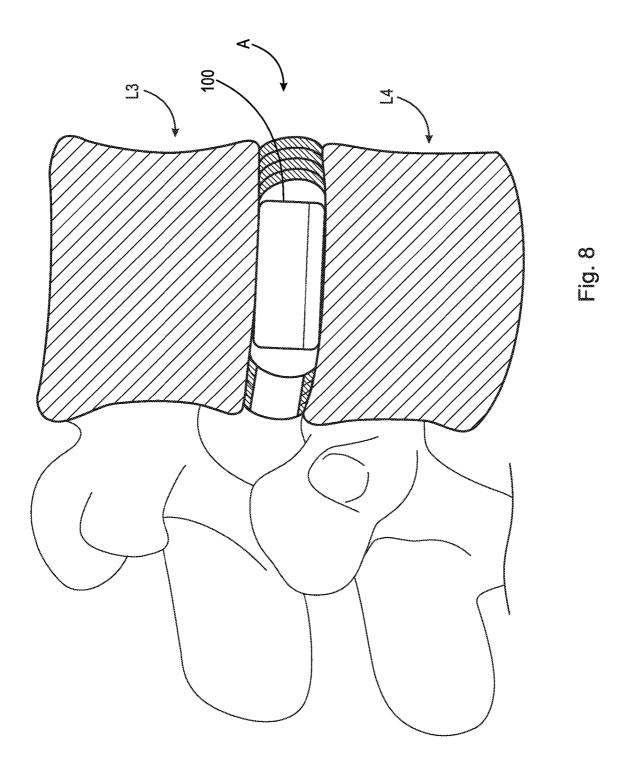
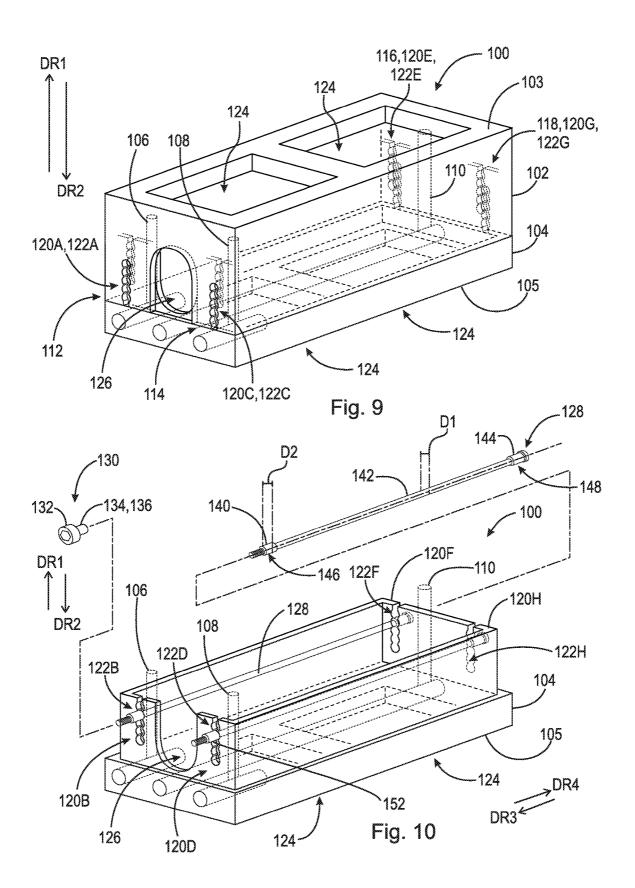


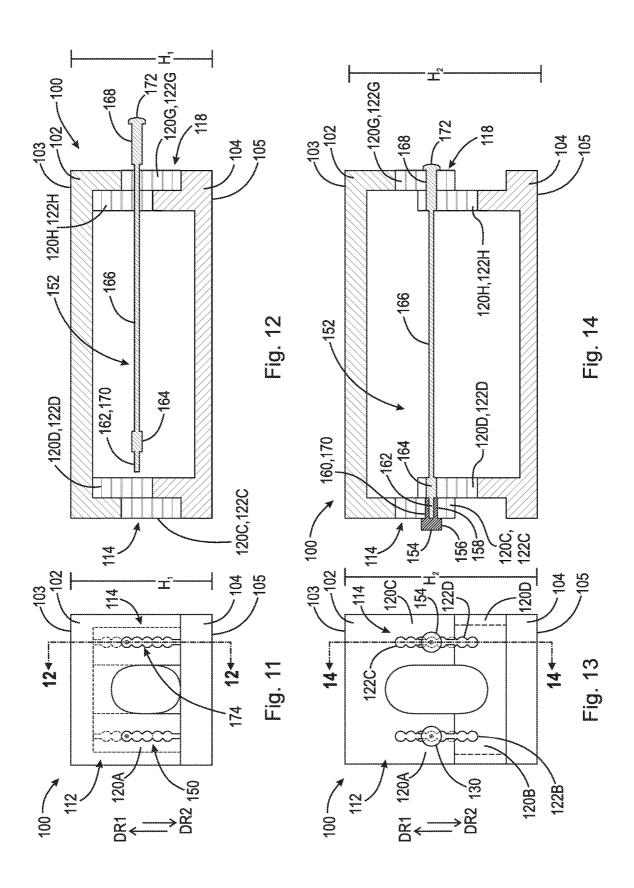
Fig. 5

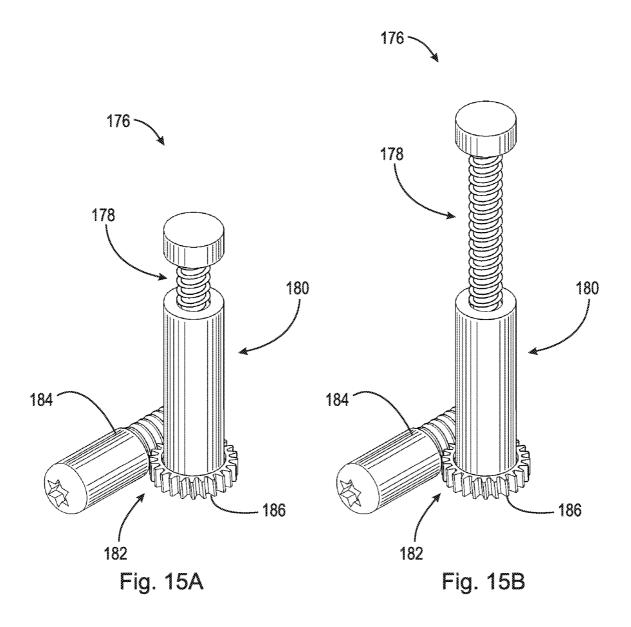












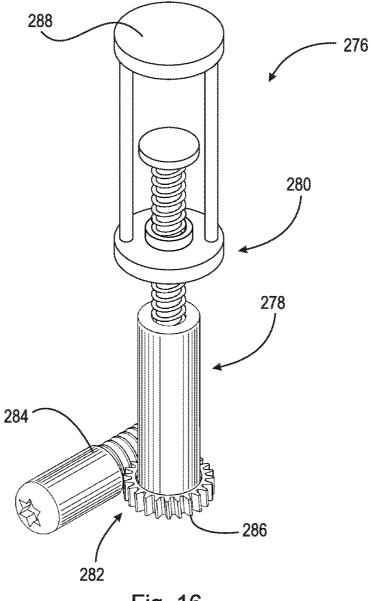
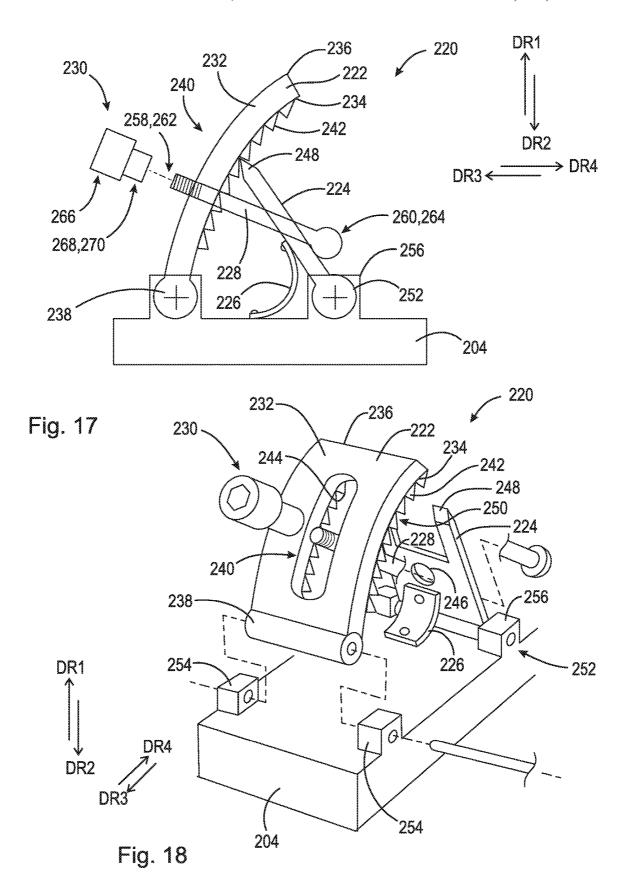
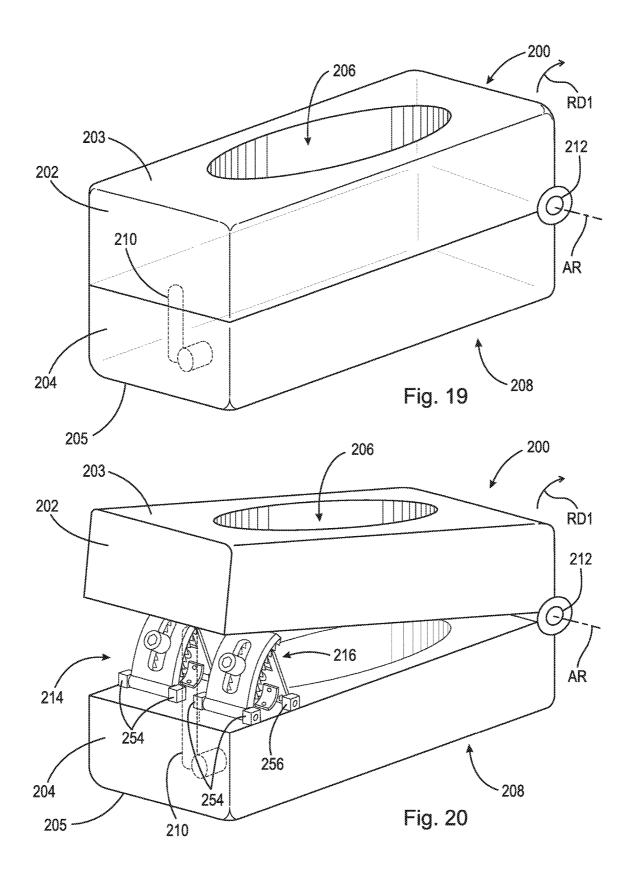
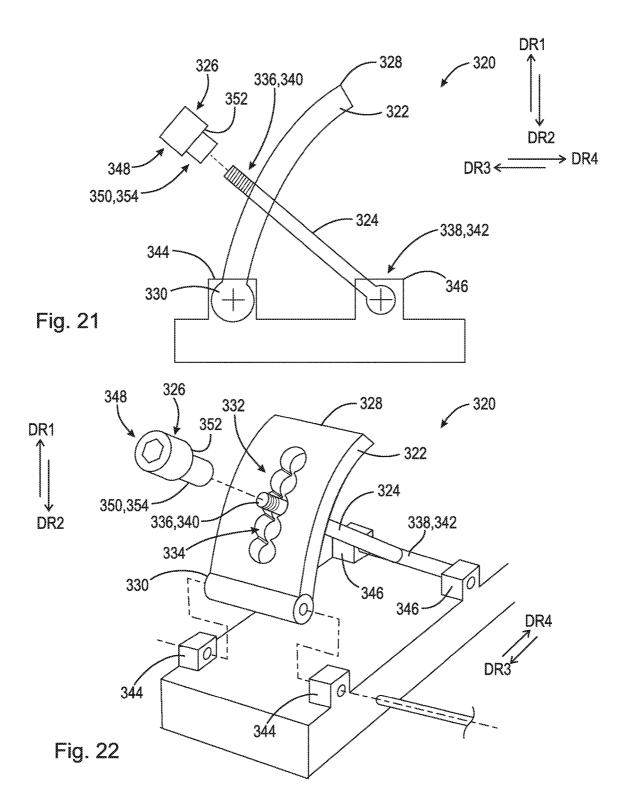
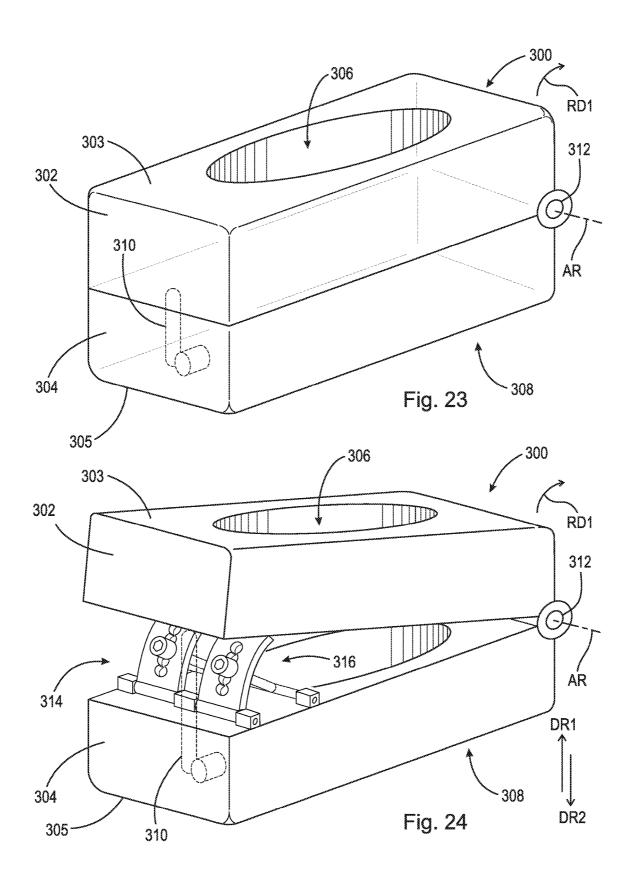


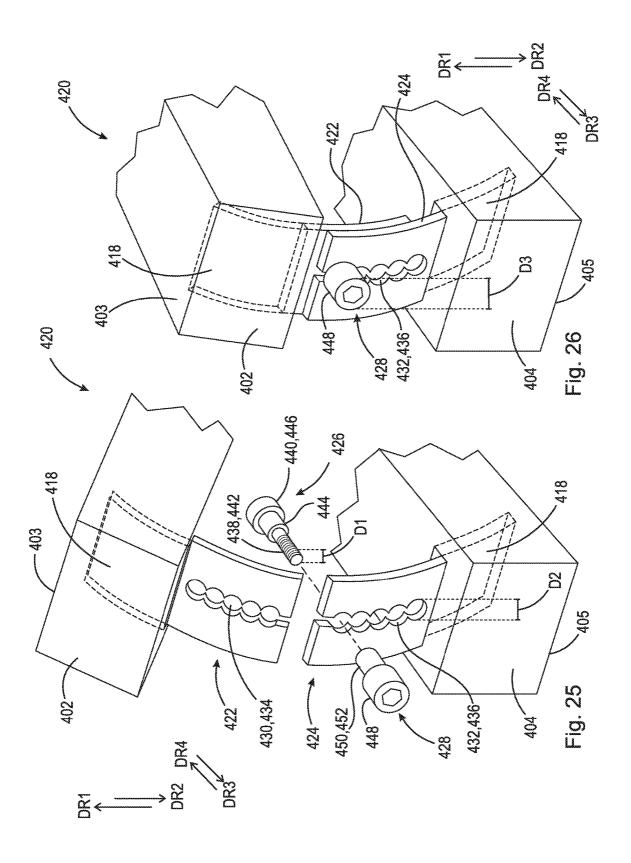
Fig. 16

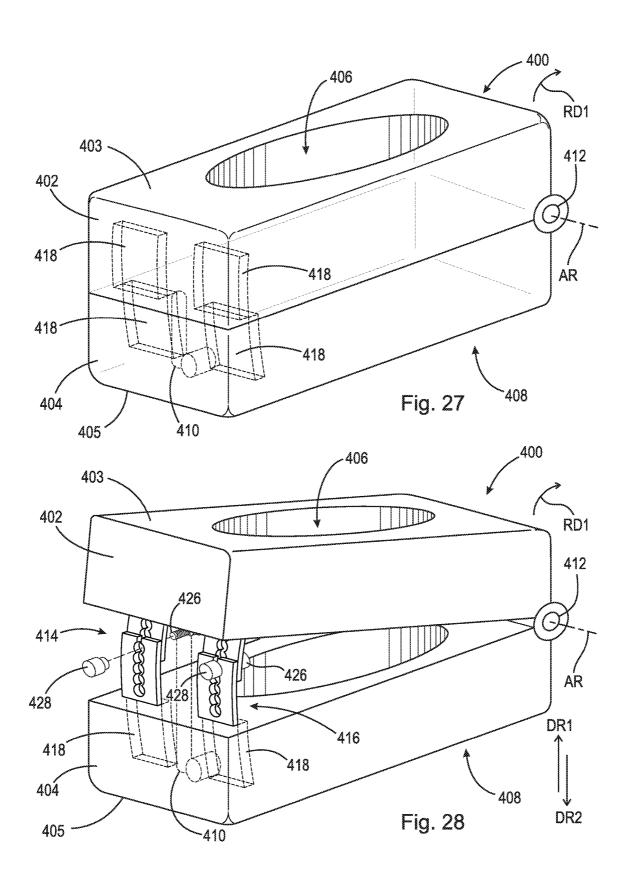


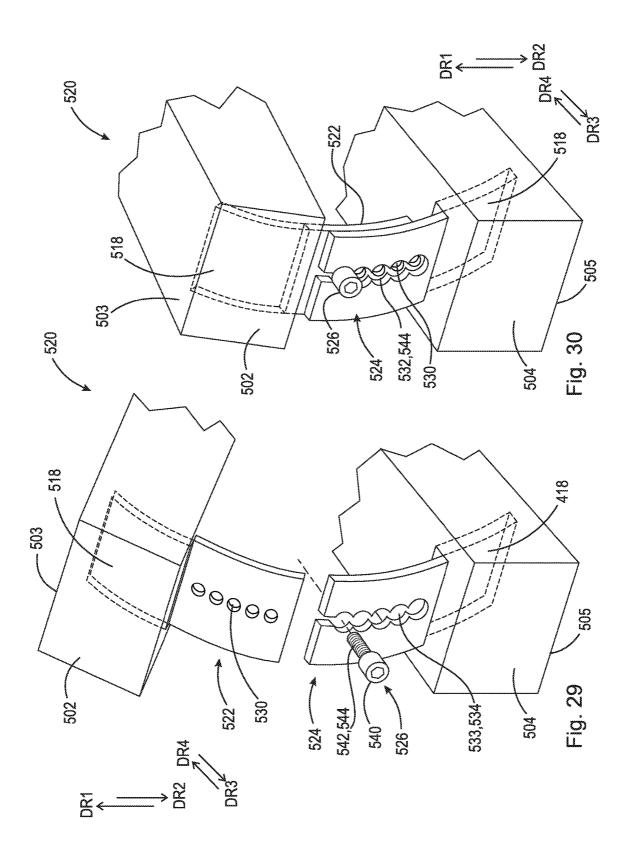


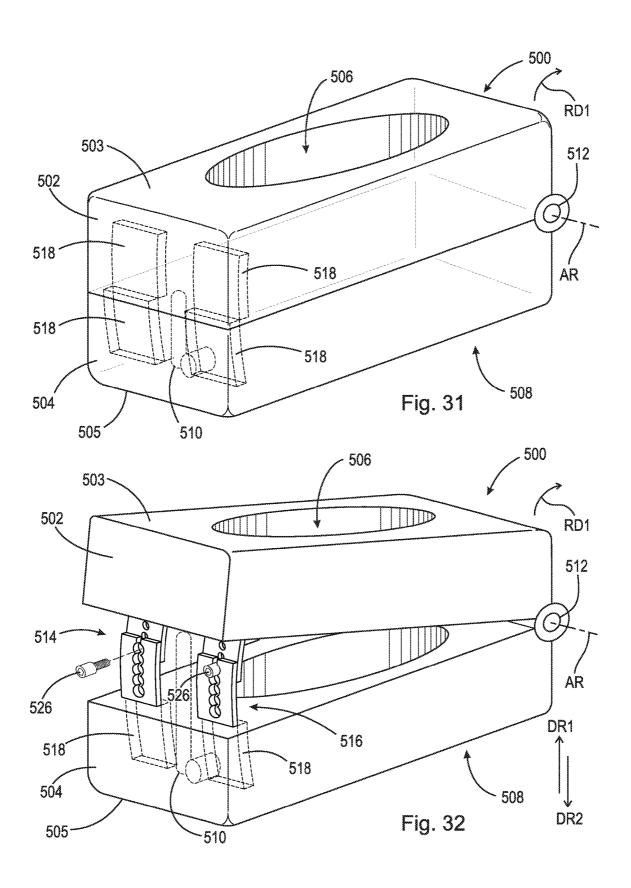


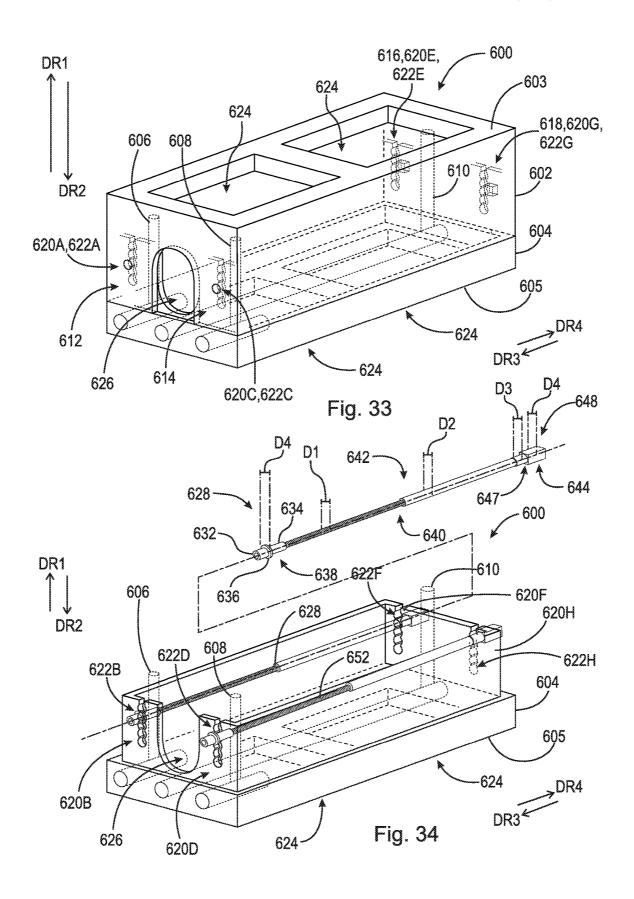


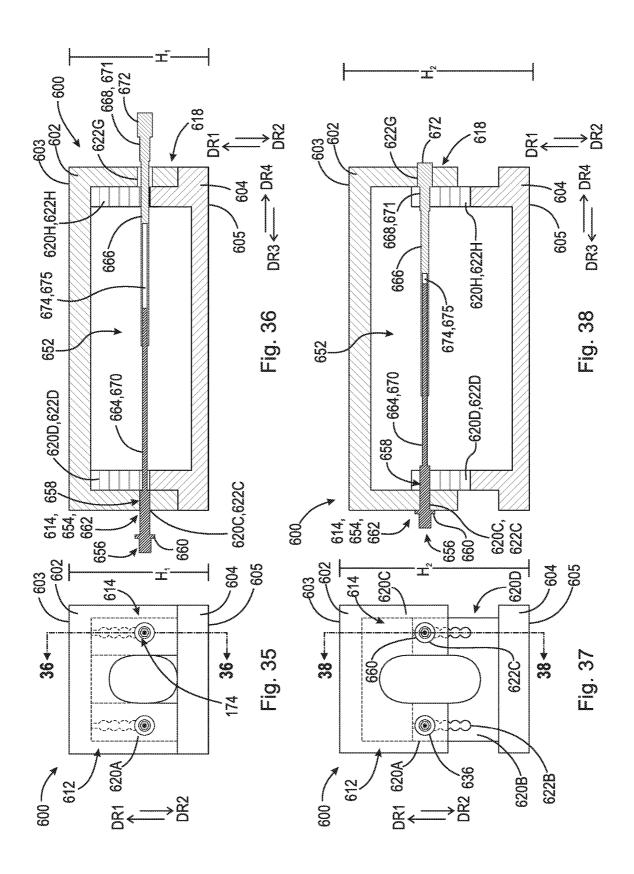


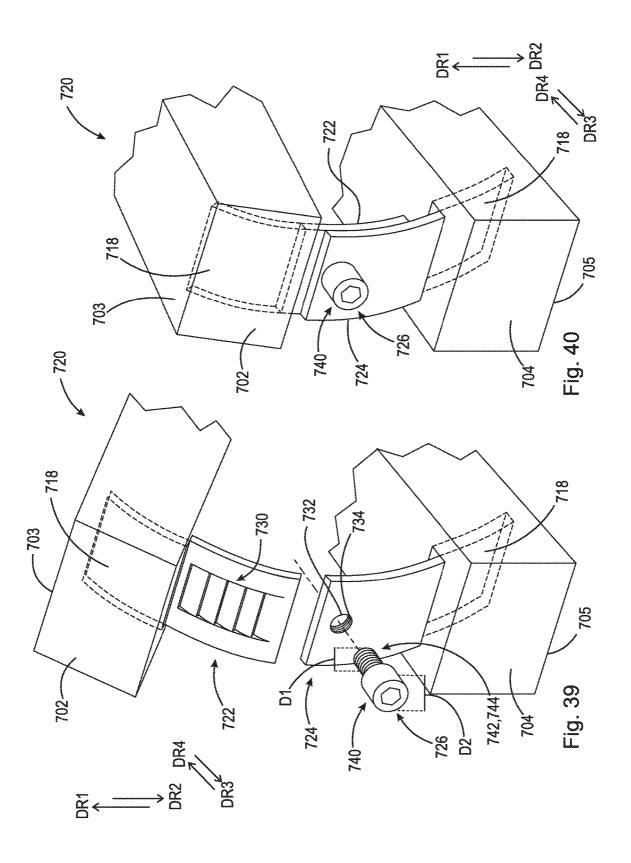


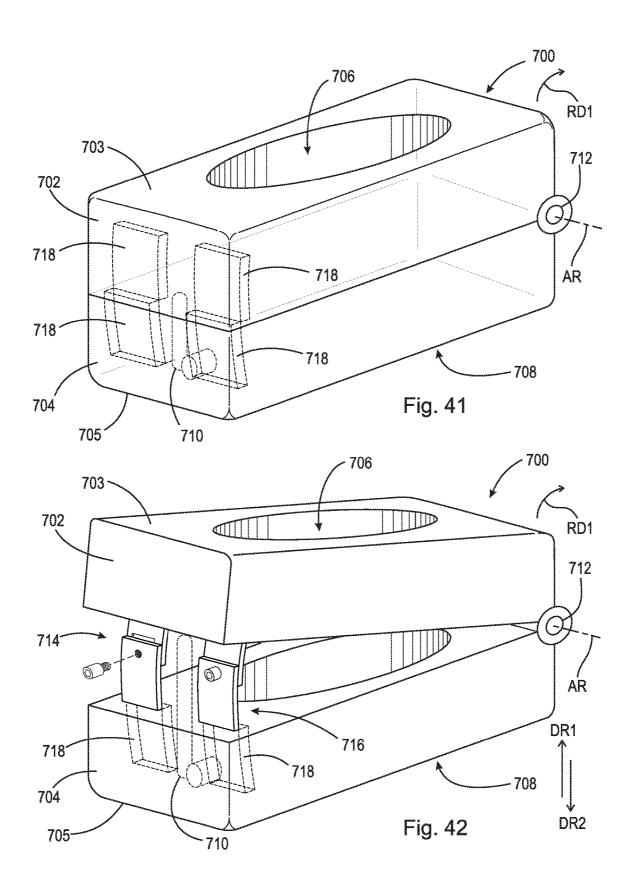


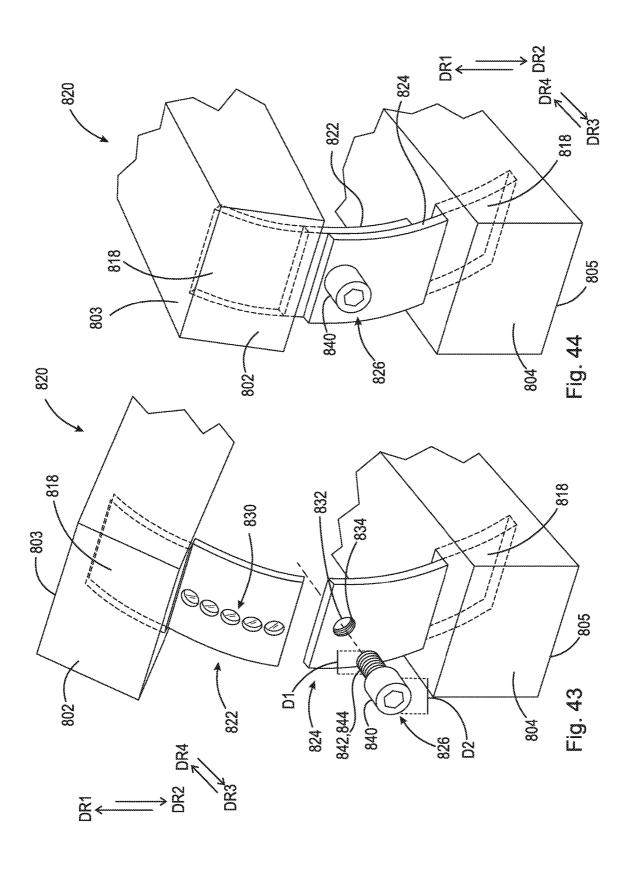


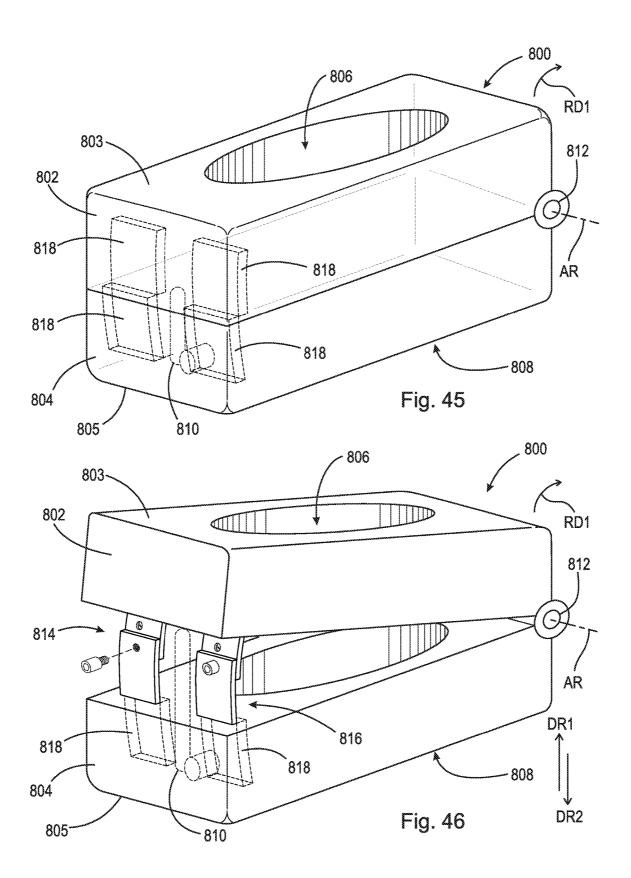












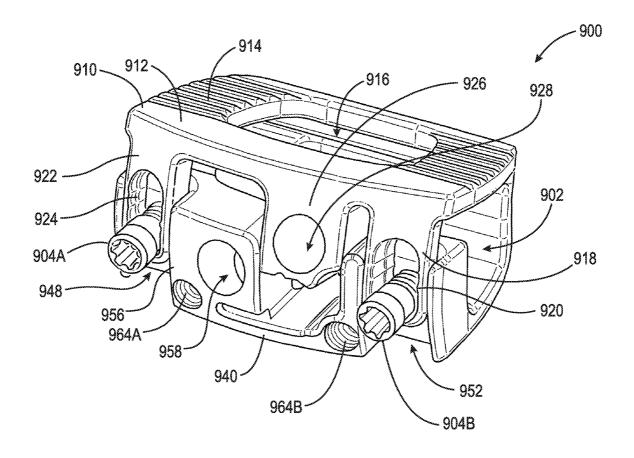


Fig. 47

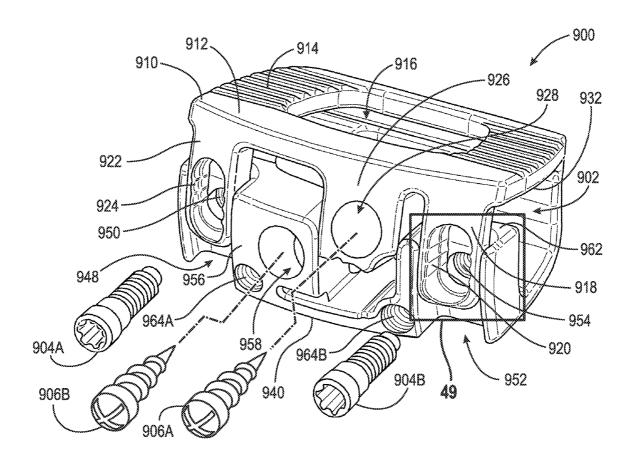


Fig. 48

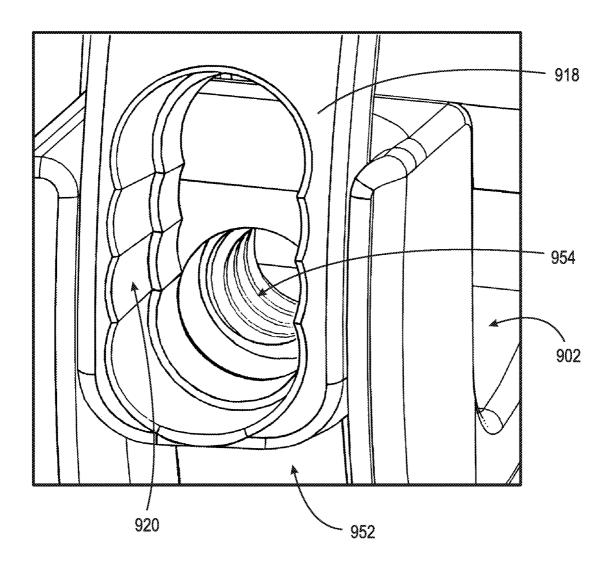


Fig. 49

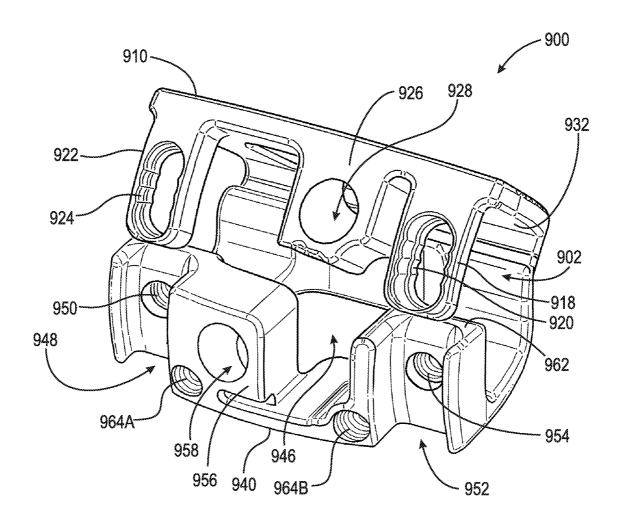


Fig. 50A

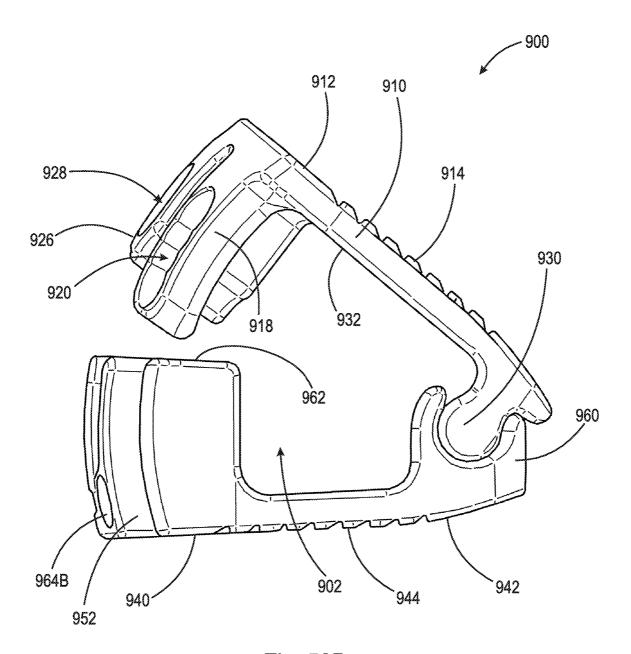


Fig. 50B

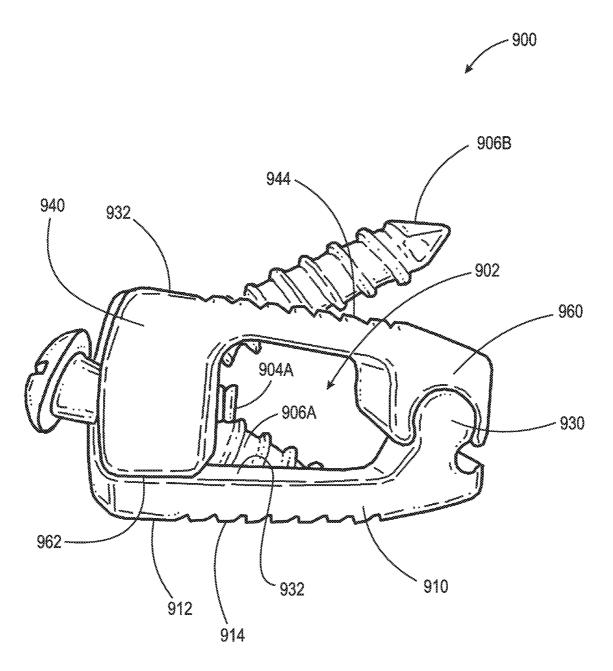


Fig. 51

STAND-ALONE EXPANDABLE INTERBODY SPINAL FUSION DEVICE WITH LOCKING MECHANISM

CROSS-REFERENCE TO RELATED APPLICATIONS

This application is filed under 35 U.S.C. § 120 as a continuation-in-part of U.S. patent application Ser. No. 15/707,756, filed on Sep. 18, 2017, which application is ¹⁰ hereby incorporated by reference in its entirety.

FIELD

The disclosure relates to spinal surgery, more particularly 15 to intervertebral prosthesis, and, even more specifically, to a stand-alone expandable interbody spinal fusion device with a locking mechanism.

BACKGROUND

The spinal column, or backbone, is one of the most important parts of the body. It provides the main support, allowing us to stand upright, bend, and twist. As shown in FIG. 1, thirty three (33) individual bones interlock with each 25 other to form the spinal column. The vertebrae are numbered and divided into regions. The cervical vertebrae (C1-C7) form the neck, support the head and neck, and allow nodding and shaking of the head. The thoracic vertebrae (T1-T12) join with the ribs to form the rib cage. The five lumbar 30 vertebrae (L1-L5) carry most of the weight of the upper body and provide a stable center of gravity when a person moves. Five vertebrae of the sacrum S and four of the coccyx C are fused. This comprises the back wall of the pelvis. Intervertebral discs are located between each of the 35 mobile vertebra. Intervertebral discs comprise a thick outer layer with a crisscrossing fibrous structure annulus A that surrounds a soft gel-like center, the nucleus N. Discs function like shock-absorbing springs. The annulus pulls the vertebral bodies together against the elastic resistance of the 40 gel-filled nucleus. When we bend, the nucleus acts like a ball bearing, allowing the vertebral bodies to roll over the incompressible gel. Each disc works in concert with two facet joints, forming a spinal motion segment. The biomechanical function of each pair of facet joints is to guide and 45 limit the movement of the spinal motion segment. The surfaces of the joint are coated with cartilage that helps each joint move smoothly. Directly behind the discs, the ring-like vertebral bodies create a vertical tunnel called the spinal canal or neuro canal. The spinal cord and spinal nerves pass 50 through the spinal canal, which protects them from injury. The spinal cord is the major column of nerve tissue that is connected to the brain and serves as an information superhighway between the brain and the body. The nerves in the spinal cord branch off to form pairs of nerve roots that travel through the small openings between the vertebrae and the intervertebral foramens.

The repetitive forces which act on these intervertebral discs during repetitive day-to-day activities of bending, lifting and twisting cause them to break down or degenerate 60 over time. Overt trauma or covert trauma occurring in the course of repetitive activities disproportionately affect the more highly mobile areas of the spine. Disruption of a disc's internal architecture leads to bulging, herniation or protrusion of pieces of the disc and eventual disc space collapse. 65 Resulting mechanical and chemical irritation of surrounding neural elements cause pain, attended by varying degrees of

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disability. In addition, loss of disc space height relaxes tension on the longitudinal ligaments, thereby contributing to varying degrees of spinal instability such as spinal curvature.

Neural irritation and instability resulting from severe disc damage has been treated by removing the damaged disc and fusing adjacent vertebral elements. Removal of the disc relieves the mechanical and chemical irritation of neural elements, while osseous union solves the problem of instability. For example, in one surgical procedure, known as a discectomy (or diskectomy) with interbody fusion, the surgeon removes the nucleus of the disc and replaces it with an implant. As shown in FIG. 2, it may be necessary, for example, for the surgeon to remove the nucleus of the disc between the L3 and L4 vertebrae. Disc D_{L3-L4} is shown in an enlarged view in FIG. 3. This figure also shows various anatomical structures of the spine, including facets F3A and F4A, facet joint FJ, spinous processes SP3 and SP4, transverse processes TP3A and TP4A, and intervertebral foramen IF. FIG. 4 is a top view of the section of the spinal column shown in FIG. 3, with the L3 vertebra removed to expose annulus A and nucleus N of disc D_{L3-L4} . Neural canal NC is also shown. FIG. 5 is an anterior perspective view of the section of the spinal column shown in FIG. 4. FIG. 6 is a partial cross-sectional view of the section of the spinal column shown in FIG. 5, but with vertebra L3 in place atop disc D_{L3-L4} .

While cancellous bone appears ideal to provide the biologic components necessary for osseous union to occur, it does not initially have the strength to resist the tremendous forces that may occur in the intervertebral disc space, nor does it have the capacity to adequately stabilize the spine until long term bony union occurs. For these reasons, many spinal surgeons have found that interbody fusion using bone alone has an unacceptably high rate of bone graft migration or even expulsion or nonunion due to structural failure of the bone or residual degrees of motion that retard or prohibit bony union.

Intervertebral prosthesis in various forms have therefore been used to provide immediate stability and to protect and preserve an environment that fosters growth of grafted bone such that a structurally significant bony fusion can occur.

After insertion, and shortly after the conclusion of the surgical process, these interbody devices experience the full weight of the patient's upper body, originally experienced by the disc prior to replacement. This weight may be sufficient to cause expandable intervertebral implants such as the implants disclosed in U.S. patent application Ser. No. 15/416,270 filed Jan. 26, 2017, which application is herein incorporated by reference in its entirety, to collapse from their expanded state to their unexpanded height, thereby negatively affecting the quality of bone fusion.

Thus, there is a long-felt need for a stand-alone expandable interbody spinal fusion device with a locking mechanism operatively arranged to prevent collapse of an interbody device after insertion.

SUMMARY

According to aspects illustrated herein, there is provided an expandable interbody spinal fusion device, comprising an inferior component including at least one hole, a superior component connected to the inferior component, the superior component including a plurality of catches operatively arranged to align with the at least one hole, and a locking screw operatively arranged to engage the plurality of catches

and the at least one hole to lock the superior component with respect to the inferior component.

According to aspects illustrated herein, there is provided an expandable interbody spinal fusion device, comprising an inferior component including a first surface and at least one 5 hole, a superior component hingedly connected to the inferior component, the superior component including a second surface and a plurality of catches operatively arranged to align with the at least one hole, a cavity formed between the inferior component and the superior component, and a locking screw operatively arranged to engage the plurality of catches and the at least one hole to lock the superior component with respect to the inferior component.

According to aspects illustrated herein, there is provided 15 a stand-alone expandable interbody spinal fusion device including a superior component, an inferior component, an expansion mechanism operatively arranged to displace the superior component in a first direction relative to the inferior component about a first hinge, and a locking mechanism. 20 The locking mechanism including a plate operatively arranged to pivot about a second hinge, the plate further comprising a first through-bore and a first plurality of teeth, a pawl operatively arranged to pivot about a third hinge, the pawl further comprising a second through-bore, and a post 25 operatively arranged to pass through the second and third through-bores such that after the superior component is displaced in the first direction, the locking mechanism prevents displacement of the superior component in a second direction, opposite the first direction.

According to aspects illustrated herein, there is provided a stand-alone expandable interbody spinal fusion device including a superior component, an inferior component, an expansion mechanism operatively arranged to displace the superior component in a first direction relative to the inferior component about a hinge, and a locking mechanism. The locking mechanism including a first plate fixedly secured to the superior component, the first plate further comprising a first through-bore, a second plate fixedly secured to the inferior component, the second plate further comprising a 40 second through-bore, a post having a first end and a second end such that after the superior component is displaced in the first direction, the locking mechanism prevents displacement of the superior component in a second direction, opposite the

According to aspects illustrated herein, there is provided a stand-alone expandable interbody spinal fusion device including a superior component, an inferior component, an expansion mechanism operatively arranged to displace the superior component in a first direction relative to the inferior 50 component, and a locking mechanism. The locking mechanism including a first plate fixedly secured to the superior component, the first plate further comprising a first throughbore, a second plate fixedly secured to the inferior component, the second plate further comprising a second through- 55 in an expanded state; bore, a third plate fixedly secured to the superior component, the third plate further comprising a third through-bore, a fourth plate fixedly secured to the inferior component, the fourth plate further comprising a fourth through-bore, and, a post arranged to engage with the first through-bore, the 60 second through-bore, the third through-bore, and the fourth through-bore, such that after the superior component is displaced in the first direction, the locking mechanism prevents displacement of the superior component in a second direction, opposite the first direction.

These and other objects, features, and advantages of the present disclosure will become readily apparent upon a

review of the following detailed description of the disclosure, in view of the drawings and appended claims.

BRIEF DESCRIPTION OF THE DRAWINGS

Various embodiments are disclosed, by way of example only, with reference to the accompanying schematic drawings in which corresponding reference symbols indicate corresponding parts, in which:

FIG. 1 is an anterior perspective view of spinal column

FIG. 2 is an anterior perspective view of the lumbar section of spinal column 10;

FIG. 3 is a lateral perspective view of L3, L4 vertebrae and disc D_{L3-L4} and related spinal anatomy;

FIG. 4 is a top view of a section of the spinal column, taken generally along line 4-4 in FIG. 3;

FIG. 5 is an enlarged anterior perspective view of the spinal column shown in FIG. 2, except with vertebra L3 and all other structure above L3 removed;

FIG. 6 is a partial cross-sectional view of the L4 vertebra and D_{L3-L4} disc shown in FIG. 5, including L3 in cross-

FIG. 7 is a partial cross-sectional view of the L4 vertebra and D_{L3-L4} disc shown in FIG. 5, showing the removal of the disc nucleus post-discectomy including L3 in cross-section;

FIG. 8 illustrates the introduction of the stand-alone expandable interbody spinal fusion device into the disc space in an unexpanded state;

FIG. 9 is a perspective view of a first embodiment of a stand-alone expandable interbody spinal fusion device, in an unexpanded state;

FIG. 10 is a partially-exploded perspective view of a stand-alone expandable interbody spinal fusion device with a first embodiment of a locking mechanism, in an expanded state:

FIG. 11 is a front view of a stand-alone expandable interbody spinal fusion device with a first embodiment of a locking mechanism, in an unexpanded state;

FIG. 12 is a cross-sectional view of a stand-alone expandable interbody spinal fusion device with a first embodiment of a locking mechanism, in an unexpanded state, taken generally along line 12-12 in FIG. 11;

FIG. 13 is a front view of a stand-alone expandable interbody spinal fusion device with a first embodiment of a locking mechanism, in an expanded state;

FIG. 14 is a cross-sectional view of a stand-alone expandable interbody spinal fusion device with a first embodiment of a locking mechanism, in an expanded state, taken generally along line 14-14 in FIG. 13;

FIG. 15A is a perspective view of an expansion mechanism in an unexpanded state;

FIG. 15B is a perspective view an expansion mechanism

FIG. 16 is a perspective view of an expansion mechanism; FIG. 17 is a side view of a second embodiment of a locking mechanism;

FIG. 18 is a front perspective partially exploded view of a second embodiment of a locking mechanism;

FIG. 19 is a front perspective view of a stand-alone expandable interbody spinal fusion device with a second embodiment of a locking mechanism, in an unexpanded state:

FIG. 20 is a front perspective view of a stand-alone expandable interbody spinal fusion device with a second embodiment of a locking mechanism, in an expanded state;

FIG. 21 is a side view of a third embodiment of a locking mechanism:

FIG. 22 is a front perspective partially exploded view of a third embodiment of a locking mechanism;

FIG. 23 is a front perspective view of a stand-alone ⁵ expandable interbody spinal fusion device with a third embodiment of a locking mechanism, in an unexpanded state:

FIG. **24** is a front perspective view of a stand-alone expandable interbody spinal fusion device with a third embodiment of a locking mechanism, in an expanded state;

FIG. 25 is a front perspective partial view of a fourth locking mechanism in an unlocked state;

FIG. 26 is a front perspective partial view of a fourth $_{15}$ locking mechanism in a locked state;

FIG. 27 is a front partially-exploded perspective view of a stand-alone expandable interbody spinal fusion device with a fourth embodiment of a locking mechanism in an unexpanded state;

FIG. 28 is a front perspective view of a stand-alone expandable interbody spinal fusion device with a fourth embodiment of a locking mechanism in an expanded state;

FIG. 29 is a front perspective partial view of a fifth locking mechanism in an unlocked state;

FIG. 30 is a front perspective partial view of a fifth locking mechanism in a locked state;

FIG. 31 is a front partially-exploded perspective view of a stand-alone expandable interbody spinal fusion device with a fifth embodiment of a locking mechanism in an 30 unexpanded state;

FIG. 32 is a front partially-exploded perspective view of a stand-alone expandable interbody spinal fusion device with a fifth embodiment of a locking mechanism in an expanded state;

FIG. 33 is a perspective view of a sixth embodiment of a stand-alone expandable interbody spinal fusion device, in an unexpanded state;

FIG. **34** is a partially-exploded perspective view of a stand-alone expandable interbody spinal fusion device with 40 a sixth embodiment of a locking mechanism, in an expanded state;

FIG. **35** is a front view of a stand-alone expandable interbody spinal fusion device with a sixth embodiment of a locking mechanism, in an unexpanded state;

FIG. 36 is a cross-sectional view of a stand-alone expandable interbody spinal fusion device with a sixth embodiment of a locking mechanism, in an unexpanded state, taken generally along line 36-36 in FIG. 35;

FIG. 37 is a front view of a stand-alone expandable 50 interbody spinal fusion device with a sixth embodiment of a locking mechanism, in an expanded state;

FIG. 38 is a cross-sectional view of a stand-alone expandable interbody spinal fusion device with a sixth embodiment of a locking mechanism, in an expanded state, taken generally along line 38-38 in FIG. 37;

FIG. 39 is a front perspective partial view of a seventh embodiment of a locking mechanism in an unlocked state;

FIG. **40** is a front perspective partial view of a seventh embodiment of a locking mechanism in a locked state;

FIG. 41 is a front partially-exploded perspective view of a stand-alone expandable interbody spinal fusion device with a seventh embodiment of a locking mechanism in an unexpanded state;

FIG. **42** is a front perspective view of a stand-alone 65 expandable interbody spinal fusion device with a seventh embodiment of a locking mechanism in an expanded state;

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FIG. 43 is a front perspective partial view of an eighth embodiment of a locking mechanism in an unlocked state;

FIG. 44 is a front perspective partial view of an eighth embodiment of a locking mechanism in a locked state;

FIG. **45** is a front partially-exploded perspective view of a stand-alone expandable interbody spinal fusion device with an eighth embodiment of a locking mechanism in an unexpanded state;

FIG. **46** is a front perspective view of a stand-alone expandable interbody spinal fusion device with an eighth embodiment of a locking mechanism in an expanded state;

FIG. 47 is a front perspective view of a stand-alone expandable interbody spinal fusion device in an expanded state:

FIG. **48** is a partial exploded view of the stand-alone expandable interbody spinal fusion device shown in FIG. **47**.

FIG. **49** is a detail view of the stand-alone expandable interbody spinal fusion device taken generally along detail **49** in FIG. **48**;

FIG. **50**A is a front perspective view of the stand-alone expandable interbody spinal fusion device shown in FIG. **47**;

FIG. **50**B is a side elevational view of the stand-aloneexpandable interbody spinal fusion device shown in FIG. **50**A; and,

FIG. **51** is a side elevational view of the stand-alone expandable interbody spinal fusion device shown in FIG. **47** in a collapsed state.

DETAILED DESCRIPTION

At the outset, it should be appreciated that like drawing numbers on different drawing views identify identical, or functionally similar, structural elements. It is to be understood that the claims are not limited to the disclosed aspects.

Furthermore, it is understood that this disclosure is not limited to the particular methodology, materials and modifications described and as such may, of course, vary. It is also understood that the terminology used herein is for the purpose of describing particular aspects only, and is not intended to limit the scope of the claims.

Unless defined otherwise, all technical and scientific terms used herein have the same meaning as commonly understood to one of ordinary skill in the art to which this disclosure pertains. It should be understood that any methods, devices or materials similar or equivalent to those described herein can be used in the practice or testing of the example embodiments. The assembly of the present disclosure could be driven by hydraulics, electronics, pneumatics, and/or springs.

It should be appreciated that the term "substantially" is synonymous with terms such as "nearly," "very nearly," "about," "approximately," "around," "bordering on," "close to," "essentially," "in the neighborhood of," "in the vicinity of," etc., and such terms may be used interchangeably as appearing in the specification and claims. It should be appreciated that the term "proximate" is synonymous with terms such as "nearby," "close," "adjacent," "neighboring," "immediate," "adjoining," etc., and such terms may be used interchangeably as appearing in the specification and claims. The term "approximately" is intended to mean values within ten percent of the specified value.

The term "superior component" as used in the present disclosure is intended to mean the component of the body of the implant located in the highest position relative to the other components in first direction DR1.

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The term "inferior component" as used in the present disclosure is intended to mean the component of the body of the implant located in the lowest position relative to the other components in first direction DR1.

The term "gear shaft" as used in the present disclosure is 5 intended to mean any gear currently understood in the art that has been elongated such that it is substantially cylindrical in shape.

The term "pawl" as used in the present disclosure is intended to mean a plate or bar having one end arranged to 10 engage the teeth of a ratchet and place pressure on the ratchet in a first direction such that the ratchet can only be disengaged from the teeth by motion in a second direction, opposite the first direction.

Adverting now to the Figures, and as described previ- 15 ously, FIGS. **1-6** depict various parts and sections of spinal anatomy. FIG. **7** illustrates a partial cross-sectional view of the L3 and L4 vertebra with disc D_{L3-L4} removed (post discectomy) and able to receive stand-alone expandable interbody spinal fusion device **100**.

FIG. 8 illustrates a partial cross-sectional view of the L3 and L4 vertebra with stand-alone expandable interbody spinal fusion device 100 in place within disc space 12 in an unexpanded state.

FIG. 9 is a perspective view of stand-alone expandable 25 interbody spinal fusion device 100, in an unexpanded state. Device 100 comprises superior component 102, inferior component 104, and expansion mechanisms 106, 108, and 110 (described infra) arranged to displace superior component 102 in a first direction DR1 relative to inferior component 104, giving device 100 an expanded height H_2 greater than unexpanded height H_1 (shown in FIGS. 11 and 13). Device 100 also comprises locking mechanisms 112, 114, 116, and 118 arranged between superior component 102 and inferior component 104 (locking mechanisms 116 and 118 are shown in FIG. 10).

Locking mechanism 112 comprises plates 120A (shown in FIG. 9) and 120B (shown in FIG. 10). Locking mechanism 114 comprises plates 120C (shown in FIG. 9) and 120D (shown in FIG. 10). Locking mechanism 116 comprises plates 120E (shown in FIG. 9) and 120F (shown in FIG. 10). Locking mechanism 118 comprises plates 120G (shown in FIG. 9) and 120H (shown in FIG. 10). Each of plates 120A-120H further include a plurality of throughbores, i.e., plurality of throughbores 122A-122H, respectively. It should be appreciated that, although plates 120A-120H are shown as integral within superior component 102 and inferior component 104, plates 120A-120H could also be discrete plates, fixedly secured to superior component 102 and inferior component 104.

Superior component 102 and inferior component 104 further comprise at least one first aperture 124 arranged to allow fusion between bone fusing material and the adjacent vertebra and a second aperture 126 located on the front face of device 100 and arranged to allow the introduction of bone 55 fusing material into device 100. Second aperture 126 is illustrated as an arched slot as a non-limiting example, however, it should be appreciated that second aperture 126 could be an aperture of any suitable shape, e.g., triangular, circular, rectangular, elliptical, etc., that would allow for the 60 introduction of bone fusing material into device 100. Superior component 102 has a first surface 103 and inferior component 104 has a first surface 105.

FIG. 10 is a perspective view of stand-alone expandable interbody spinal fusion device 100, in an expanded state. It 65 should be appreciated that FIG. 10 is a partial view, i.e., superior component 102 has been removed for clarity.

During surgery and after device 100 is implanted in disc space 12, a surgeon can apply torque to expansion mechanisms 106, 108, and 110 via any device that imparts rotational force upon expansion mechanisms 106, 108, and 110 (e.g., a screw driver or impact driver). Expansion mechanisms 106, 108 and 110 are preferably the embodiment

illustrated in FIGS. 15 and 16, described infra. Furthermore, it should be appreciated that although expansion mechanisms 106, 108, and 110 are depicted within inferior component 104 in FIGS. 9-14, expansion mechanisms 106, 108, and 110 could be arranged within superior component 102. This rotational force causes expansion mechanisms 106,

108, and 110, to displace superior component 102 in direction DR1 relative to inferior component 104 giving device 100 an expanded height H₂, greater than H₁ (shown in FIGS. 11 and 13). It should be appreciated that expansion mecha-

nisms 106, 108, and 110 can be expanded to any height between unexpanded height H_1 and expanded height H_2 . Device 100 further comprises post 128 and fastener 130. Post 128 and fastener 130 are provided to secure locking

mechanisms 112 and 116 in position once device 100 is expanded to its final height. Fastener 130 has a first end 132 and a second end 134. First end 132 is operatively arranged to engage with any device known in the art that can impart

5 rotational motion onto fastener 130, e.g., a drill. Second end 134 includes female threading 136. Post 128 further includes four sections, i.e., section 138, section 140, section 142, and section 144. Section 138 comprises male threading 146

operatively arranged to engage with female threading 136. Section 144 comprises stopping element 148. It should be appreciated that, although stopping element 148 is depicted as a flanged member, other variations of stopping elements

can be used, e.g., a spherical stopping element. Sections 138 and 142 have diameter D1 and sections 140 and 144 have diameter D2, where D2 is greater than D1. Prior to locking, sections 138 and 142 having diameter D1 are loosely seated in longitudinal space 150 (shown in FIG. 11) arranged

between each through-bore in the plurality of through-bores 122A, 122B, 122E, and 122F. After device 100 has been inserted into disc space 12 and expanded to an appropriate height, a surgeon can apply torque to first end 132 of fastener 130, pulling post 128 in direction DR3 into the locked position. In the locked position, sections 140 and 144 are

completely seated in one of the through-bores of plurality of through-bores 122A, 122B, 122E, and 122F, which correspond to the chosen device height. In this locked position, device 100 is prevented from collapsing in direction DR2.

Device 100 further comprises post 152 and fastener 154 (shown in FIG. 14). Post 152 and fastener 154 are provided to secure locking mechanisms 114 and 118 in position once device 100 is expanded to its final height. Fastener 154 has a first end 156 and a second end 158. First end 156 includes a recess operatively arranged to engage with any device known in the art that can impart rotational motion onto fastener 154, e.g., a drill. Second end 158 includes female threading 160. Post 152 includes four sections, i.e., section 162, section 164, section 166, and section 168. Section 162 comprises male threading 170 operatively arranged to engage with female threading 160 of fastener 154. Section 168 comprises stopping element 172. It should be appreciated that, although stopping element 172 is depicted as a flanged member, other variations of stopping elements can be used, e.g., a spherical stopping element. Sections 162 and 166 have diameter D1 and sections 164 and 168 have diameter D2 where D2 is greater than D1. Prior to locking, sections 162 and 166, having diameter D1, are loosely seated in longitudinal space 174 (shown in FIG. 11) arranged

between each through-bore in the plurality of through-bores 122C, 122D, 122G, and 122H. After device 100 has been inserted into disc space 12 and expanded to an appropriate height, a surgeon can apply torque to first end 156 of fastener 154, pulling post 152 in direction DR3 into the locked position. In the locked position, sections 164 and 168 are seated in one of the through-bores of plurality of through-bores 122C, 122D, 122G, and 122H, which corresponds to the chosen device height. In this locked position, device 100 is prevented from collapsing in direction DR2.

FIG. 11 is a front view of stand-alone expandable interbody spinal fusion device 100, in an unexpanded state having an unexpanded height H₁. FIG. 12 is a crosssectional view of stand-alone expandable interbody spinal fusion device 100, in an unexpanded state having an unex- 15 panded height H₁. FIG. 13 is a front view stand-alone expandable interbody spinal fusion device 100, in an expanded state having an expanded height H2, greater than H₁. FIG. 14 is a cross-sectional view of stand-alone expandable interbody spinal fusion device 100 in an expanded state 20 having an expanded height H₂, greater than H₁. It should be appreciated that in FIGS. 12 and 14, expansion mechanisms 106, 108 and 110 have been removed for clarity. It should also be appreciated that, although pluralities of throughbores 122A-122H are illustrated with a longitudinal space 25 between each through-bore of each plurality of throughbores, it is also contemplated that plurality of through-bores 122A-122H could include multiple discrete through-bores, separate and distinct from each other with no longitudinal space between them.

FIG. 15A is a perspective view of expansion mechanism 176 in an unexpanded state. FIG. 15B is a perspective view of an expansion mechanism 176 in an expanded state. Expansion mechanism 176 comprises threaded rod 178, threaded sleeve 180, and worm drive 182 having worm 184 and gear 186. A portion of threaded rod 178 can be embedded within superior component 102 such that it is rotationally fixed; however, it should be appreciated that the frictional engagement between the top surface of threaded rod 178 and the inner surface of superior component 102 may be 40 sufficient to prevent threaded rod 178 from freely rotating. During surgery and after device 100 is implanted in disc space 12, a surgeon can apply torque to worm drive 182 via any device that imparts rotational force upon worm 184 (e.g., a screw driver or impact driver). Torque is transferred 45 90 degrees through worm drive 182, via worm 184 and gear 186. Rotation of gear 186 causes threaded sleeve 180 to rotate. As threaded sleeve 180 rotates, threaded rod 178 remains rotationally locked due to the portion embedded within superior component 102, or frictional contact with 50 the inner surface of superior component 102. As threaded sleeve 180 rotates, the threads of the rotationally locked threaded rod 178 ride upward along the threads within threaded sleeve 180, displacing threaded rod 178, and subsequently superior component 102, in direction DR1. 55 Threaded rod 178 includes a stopping feature to prevent threaded rod 178 from being ejected from threaded sleeve 180. For example, the lower portion of threaded rod 178 could be threadless (not shown in the figures), and therefore prevent threaded rod 178 from being ejected from threaded 60 sleeve 180. When threaded rod 178 reaches its maximum expansion, the unthreaded portion of threaded rod 178 remains within threaded sleeve 180, preventing threaded rod 178 from being pushed out of threaded sleeve 180. Alternatively, the stopping feature could be a flange on the 65 recessed portion of threaded rod 178 arranged to engage with a retention shoulder (not shown in the figures) within

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threaded sleeve **180** in a fully expanded state. It should be appreciated that worm drive **182** could be arranged to transfer torque in other arrangements, i.e., 180 degrees, 270 degrees, or any desirable angle required by the arrangement of worm **184** and gear **186**. It should further be appreciated that although a gear **186** is depicted in the figures as a spur gear, other suitable gears may be selected, i.e., a bevel gear, a hypoid gear, a spiral gear, or a face gear.

FIG. 16 is a perspective view of expansion mechanism 10 276. Expansion mechanism 276 comprises threaded rod 278, lifting nut 280, and worm drive 282 having worm 284 and gear 286. Lifting nut 280 may be connected to superior component 102. In some embodiments, lifting nut 280 comprises platform 288 connected thereto, wherein the platform 288 is connected to superior component 102 such that lifting nut 280 is rotationally fixed. Lifting nut 280 may be fixedly secured to superior component 102; however, it should be appreciated that the frictional engagement between platform 288 and the inner surface of superior component 102 may be sufficient to prevent lifting nut 280 from freely rotating. During surgery and after device 100 is implanted in disc space 12, a surgeon can apply torque to worm drive 282 via any device that imparts rotational force upon worm 284 (e.g., a screw driver or impact driver). Torque is transferred 90 degrees through worm drive 282, via worm 284 and gear 126. Rotation of gear 286 causes threaded rod 278 to rotate. Threaded rod 278 is nonrotatably connected to gear 286. As threaded rod 278 rotates, lifting nut 280 remains rotationally locked due to platform 288 being embedded within superior component 102, or frictional contact with the inner surface of superior component 102. As threaded rod 278 rotates, the threads of the rotationally locked lifting nut 280 ride upward along the threads on threaded rod 278, displacing lifting nut 280, and subsequently superior component 102, in direction DR1. Threaded rod 278 may include a stopping feature to prevent lifting nut 280 from being ejected from threaded rod 280. For example, the top portion of threaded rod 278 could be threadless (not shown in the figures), and therefore prevent lifting nut 280 from being ejected from threaded rod 278. When lifting nut 280 reaches its maximum expansion, the unthreaded portion of threaded rod 278 remains within lifting nut 280, preventing lifting nut 280 from being pushed off of threaded rod 278. Alternatively, the stopping feature could be a flange on the end of threaded rod 278 arranged to engage with lifting nut 280, as shown. It should be appreciated that worm drive 182 could be arranged to transfer torque in other arrangements, i.e., 180 degrees, 270 degrees, or any desirable angle required by the arrangement of worm 184 and gear 186. It should further be appreciated that although a gear 186 is depicted in the figures as a spur gear, other suitable gears may be selected, i.e., a bevel gear, a hypoid gear, a spiral gear, or a face gear.

FIG. 17 is a side view of locking mechanism 220. Locking mechanism 220 comprises plate 222, pawl 224, biasing element 226, post 228, and fastener 230. Plate 222 includes first surface 232, second surface 234, corner 236, hinge 238, and through-bore 240 operatively arranged to receive post 228 and fastener 230. When in the locked position, corner 236 abuts superior component 102 to stop superior component 102 from being displaced in direction DR2. Second surface 234 comprises first plurality of teeth 242 and second plurality of teeth 244. Pawl 224 includes through-bore 246, first pawl head 248, second pawl head 250, and hinge 252. Through-bore 246 is operatively arranged to accept post 228. First and second pawl heads 248 and 250 taper to a point and are operatively arranged to engage with first and

second plurality of teeth 242 and 244, respectively, on second surface 234 of plate 222. Prior to locking, plate 222 and pawl 224 are freely pivotable about hinges 238 and 252, respectively. Hinges 238 and 252 are pivotably secured to first protrusion 254 and second protrusion 256 of inferior component 204 (discussed infra), respectively. It should be appreciated that although hinges 238 and 252 are illustrated as pivotably secured to first protrusion 254 and second protrusion 256, respectively, hinges 238 and 252 could also be placed in a recess within inferior component 204. Biasing 10 element 226 is fixedly secured between inferior component 204 and pawl 224 and provides spring bias to pawl 224 in direction DR1 and/or DR4. It should be appreciated that, although biasing element 226 is depicted in FIGS. 17-20 as a flat spring, other biasing elements known in the art can be 15 used to bias pawl 224 in direction DR1. Post 228 includes first end 258 and second end 260. First end 258 includes male threading 262, and second end 260 includes a stopping element 264. It should be appreciated that, although stopping element 264 is depicted as a spherical member, other 20 variations of stopping elements can be used, e.g., a flanged stopping element. Fastener 230 includes first end 266 and second end 268. First end 266 is operatively arranged to engage with any device known in the art that can impart rotational motion onto fastener 230, e.g., a drill. Second end 25 268 includes female threading 270 operatively arranged to engage with male threading 262 of post 228.

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After device 200 has been inserted into disc space 12 and expanded to an appropriate height, a surgeon can apply torque to first end 266 of fastener 230, pulling post 228 in 30 direction DR3. As post 228 is pulled in direction DR3, stopping element 264 of post 228 forces pawl 224 in direction DR3 against biasing element 226 about hinge 252. When sufficient force is applied, first and second pawl heads 248 and 250, respectively, engage with first and second 35 plurality of teeth 242 and 244 locking the plate 222 in place and preventing the collapse of device 200 (shown in FIGS. 19 and 20) in direction DR2.

FIG. 19 is a front perspective view of device 200 having two locking mechanisms 214 and 216 in an unexpanded 40 state. It should be appreciated that in an example embodiment locking mechanisms 214 and 216 are embodied as locking mechanism 220 discussed supra. Device 200 comprises superior component 202, inferior component 204, and expansion mechanism 210 arranged to displace superior 45 component 202 in first direction DR1 relative to inferior component 204. Superior component 202 and inferior component 204 further comprise at least one first aperture 206 and at least one second aperture 208, respectively, which are arranged to allow fusion between bone fusing material and 50 the adjacent vertebra. Superior component 202 has a first surface 203 and inferior component 204 has a first surface 205. Device 200 further comprises hinge 212 fixedly secured to superior component 202 and inferior component 204 and arranged to rotatably displace the superior compo- 55 nent about axis of rotation AR. Expansion mechanism 210 is preferably expansion mechanism 176 described supra. Although FIGS. 19 and 20 depict expansion mechanism 210 fixedly secured within inferior component 204, it should be appreciated that expansion mechanism 210 could also be 60 fixedly secured within superior component 202.

FIG. 20 is a front perspective view of device 200 having locking mechanisms 214 and 216 in an expanded state. After superior component 202 is displaced about axis of rotation AR, locking mechanisms 214 and 216 are engaged and 65 locked as discussed supra. Once locked, superior component 202 is prevented from moving in direction DR2.

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FIG. 21 is a side view of locking mechanism 320. Locking mechanism 320 comprises plate 322, post 324, and fastener 326. Plate 322 includes corner 328, hinge 330, and plurality of through-bores 332 operatively arranged to receive post 324 and fastener 326. When in the locked position, corner 328 abuts superior component 102 to stop superior component 102 from being displaced in direction DR2. Post 324 includes first end 336 and second end 338. First end 336 includes male threading 340, and second end 338 includes hinge 342. Plurality of through-bores 332 (illustrated in FIG. 22) further includes longitudinal space 334 arranged to receive first end 336 of post 324. Before locking, plate 322 and post 324 are freely pivotable about hinges 330 and 342, respectively, and first end 336 of post 324 moves freely within longitudinal space 334 (shown in FIG. 22) of plurality of through-bores 332. Hinges 330 and 342 are pivotably secured to first protrusion 344 and second protrusion 346, respectively, of inferior component 302 (discussed infra). It should be appreciated that although hinges 330 and 342 are illustrated as pivotably secured to first protrusion 344 and second protrusion 346, respectively, hinges 330 and 342 could also be placed in a recess within inferior component 304. Fastener 326 includes first end 348, second end 350, and flange 352. First end 348 is operatively arranged to engage with any device known in the art that can impart rotational motion onto fastener 326, e.g., a drill. Second end 350 includes female threading 354 operatively arranged to engage with male threading 340 of post 324. Flange 352 has diameter D1 and is operatively arranged to abut against the surface of plate 322 when second end 350 is seated within one of plurality of through-bores 332 of plate 322.

After device 300 (shown in FIGS. 23 and 24) has been inserted into disc space 12 and expanded to an appropriate height, a surgeon can apply torque to first end 348 of fastener 326, pulling fastener 326 in direction DR4. As fastener 326 is pulled in direction DR4, flange 352 also moves in direction DR4 until flange 352 abuts the surface of plate 322 while second end 350 of fastener 326 is seated within one of plurality of through-bores 332 of plate 322 locking plate 322 in place and preventing the collapse of device 300 (shown in FIGS. 23 and 24) in direction DR2.

FIG. 23 is a front perspective view of device 300 with locking mechanisms 314 and 316, in an unexpanded state. It should be appreciated that in an example embodiment, locking mechanisms 314 and 316 are embodied as locking mechanism 320 discussed supra. Device 300 comprises superior component 302, inferior component 304, and expansion mechanism 310 arranged to displace superior component 302 in a first direction DR1 relative to inferior component 304. Superior component 302 and inferior component 304 further comprise at least one first aperture 306 and at least one second aperture 308, respectively, which are arranged to allow fusion between bone fusing material and the adjacent vertebra. Superior component 302 has a first surface 303 and inferior component 304 has a first surface 305. Device 300 further comprises hinge 312 fixedly secured to superior component 302 and inferior component 304 and arranged to rotatably displace the superior component about axis of rotation AR. Although FIGS. 23 and 24 depict expansion mechanism 310 fixedly secured within inferior component 304, it should be appreciated that expansion mechanism 310 could also be fixedly secured within superior component 302.

FIG. 24 is a front perspective view device 300 with locking mechanisms 314 and 316, in an expanded state. After superior component 302 is displaced about axis of rotation AR, locking mechanisms 314 and 316 are engaged

and locked as discussed supra. Once locked, superior component 302 is prevented from moving in direction DR2.

FIG. 25 is a partial front perspective view of a locking mechanism 420 in an unlocked state. Locking mechanism 420 comprises plates 422 and 424, post 426, and fastener 428. Plates 422 and 424 are fixedly secured to superior component 402 and inferior component 404 (discussed infra), respectively. Plates 422 and 424 include first plurality of through-bores 430 and second plurality of through-bores 432, respectively. First plurality of through-bores 430 and 10 second plurality of through-bores 432, which have diameter D2, less than diameter D3, and greater than diameter D1. First plurality of through-bores 430 and second plurality of through-bores 432 are operatively arranged to receive post **426** and fastener **428**. First plurality of through-bores **430** includes longitudinal space 434, and second plurality of through-bores 432 includes longitudinal space 436. Post 426 includes a first end 438 and a second end 440. First end 438 has diameter D1 and includes male threading 442, and second end 440 includes shoulder 444 and stopping element 20 446. Shoulder 444 has diameter D2 and is operatively arranged to engage with first plurality of through-bores 430. Fastener 428 includes first end 448 and second end 450. First end 448 has diameter D3 (shown in FIG. 26) and is operatively arranged to engage with any device known in the 25 art that can impart rotational motion onto fastener 428, e.g., a drill. Second end 450 has diameter D2 and includes female threading 452 operatively arranged to engage with male threading 442 of post 426.

Before locking, post 426 is freely moveable within lon- 30 gitudinal spaces 434 and 436. During surgery, and after device 400 (discussed infra) has been expanded to its final height, a surgeon imparts rotational motion to fastener 428. Female threading 452 of fastener 428 engages with male threading 442 of post 426 pulling post 426 in direction DR3. 35 Post 426 is pulled in direction DR3 until shoulder 444 engages one of the through-bores of first plurality of through-bores 430 and second end 450 of fastener 428 engages one of the through-bores of the second plurality of through-bores 432. When both second end 450 of fastener 40 428 and shoulder 444 of post 426 are engaged with the respective through-bores, device 400 is locked and is prevented from collapsing in direction DR2. It should be appreciated that, although not depicted in the figures, it is possible for shoulder 444 or second end 450 of fastener 428 45 to engage with both the first plurality of through-bores 430 and second plurality of through-bores 432 simultaneously. FIG. 26 is a partial front perspective view of a locking mechanism 420 in a locked state. When device 400 is in the fully collapsed state, plates 422 and 424 nest within recesses 50 418.

FIG. 27 is a front perspective view of device 400 with locking mechanisms 414 and 416, in an unexpanded state. Device 400 comprises superior component 402, inferior component 404, and expansion mechanism 410 arranged to 55 displace superior component 402 in a first direction DR1 relative to inferior component 404. Superior component 402 and inferior component 404 further comprise at least one first aperture 406 and at least one second aperture 408, which are arranged to allow fusion between bone fusing material and the adjacent vertebra. Superior component 402 has a first surface 403 and inferior component 404 has a first surface 405. Device 400 further comprises hinge 412 fixedly secured to superior component 402 and inferior component 404 and arranged to rotatably displace the superior component about axis of rotation AR. Locking mechanisms 414 and 416 are preferably locking mechanism 420 described

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supra. Expansion mechanism 410 is preferably expansion mechanism 176 described supra. It should be noted that since plates 422 and 424 are fixedly secured to superior and inferior components 102 and 104, respectively, recesses 418 are provided within which plates 422 and 424 can nest while device 400 is in a collapsed state. It should further be appreciated that plates 422 and 424 can be hingedly secured to superior component 402 and inferior component 404, respectively. FIG. 28 is a front perspective view of device 400 with locking mechanisms 414 and 416 in an expanded state.

FIG. 29 is a partial front perspective view of a locking mechanism 520 in an unlocked state. Locking mechanism 520 comprises plates 522 and 524, and fastener 426. Plates 522 and 524 are fixedly secured to superior component 502 and inferior component 504 (discussed infra), respectively. Plate 522 includes first plurality of through-bores 530 and plate 524 includes second plurality of through-bores 532. Each through-bore of first plurality of through-bores 530 has diameter D2. Each through-bore of the second plurality of through-bores 532 has diameter D1 larger than D2. First plurality of through-bores 530 and second plurality of through-bores 532 are operatively arranged to fastener 526. Second plurality of through-bores 532 further includes longitudinal space 534. Fastener 526 includes first end 540 and second end 542. First end 540 has diameter D2 and is operatively arranged to engage with any device known in the art that can impart rotational motion onto fastener 526, e.g., a drill. Second end 542 has diameter D1 and includes male threading 544 operatively arranged to engage with any of the through-bores of first plurality of through-bores 530.

Before locking, fastener 526 is freely moveable within longitudinal space 534. During surgery, and after device 500 (discussed infra) has been expanded to its final height, a surgeon imparts rotational motion to fastener 526. Male threading 544 of fastener 526 engages any of the throughbores of first plurality of through-bores 530 which pulls fastener 526 in direction DR4. When first end 540 of fastener 526 is engaged with second plurality of through-bores 532 and second end 542 is engaged with first plurality of through-bores 530, device 500 is locked and prevented from collapsing in direction DR2. FIG. 30 is a partial front perspective view of a locking mechanism 520 in a locked state. When device 500 is in the fully collapsed state, plates 522 and 524 nest within recesses 518.

FIG. 31 is a front perspective view of device 500 with locking mechanisms 514 and 516, in an unexpanded state. Device 500 comprises superior component 502, inferior component 504, and expansion mechanism 510 arranged to displace superior component 502 in a first direction DR1 relative to inferior component 504. Superior component 502 and inferior component 504 further comprise at least one first aperture 506 and at least one second aperture 508, which are arranged to allow fusion between bone fusing material and the adjacent vertebra. Superior component 502 has a first surface 503 and inferior component 504 has a first surface 505. Device 500 further comprises hinge 512 fixedly secured to superior component 502 and inferior component 504 and arranged to rotatably displace the superior component about axis of rotation AR. Locking mechanisms 514 and 516 are preferably locking mechanism 520 described supra. Expansion mechanism 510 is preferably expansion mechanism 176 described supra. It should be noted that since plates 522 and 524 are fixedly secured to superior and inferior components 502 and 504, respectively, recesses 518 are provided within which plates 522 and 524 can nest while device 500 is in a collapsed state. It should further be

appreciated that plates 522 and 524 can be hingedly secured to superior component 502 and inferior component 504, respectively. FIG. 32 is a front perspective view of device 500 with locking mechanisms 514 and 516 in an expanded state

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FIG. 33 is a perspective view of stand-alone expandable interbody spinal fusion device 600, in an unexpanded state. Device 600 comprises superior component 602, inferior component 604, and expansion mechanisms 606, 608, and 610 (described infra) arranged to displace superior component 602 in a first direction DR1 relative to inferior component 604, giving device 600 an expanded height H_2 greater than unexpanded height H_1 (shown in FIGS. 37 and 38). Device 600 also comprises locking mechanisms 612, 614, 616, and 618 arranged between superior component 15 602 and inferior component 604.

Locking mechanism 612 comprises plate 620A (shown in FIG. 33) and 620B (shown in FIG. 34). Locking mechanism 614 comprises plates 620C (shown in FIG. 33) and 620D (shown in FIG. 34). Locking mechanism 616 comprises 20 plates 620E (shown in FIG. 33) and 620F (shown in FIG. 34). Locking mechanism 618 comprises plates 620G (shown in FIG. 33) and 620H (shown in FIG. 34). Plates 620A and $620\mathrm{C}$ further include through-bores $622\mathrm{A}$ and $622\mathrm{C},$ respectively. tively. Plates 620E and 620G further comprise square 25 through-bores 622E and 622G, respectively. Plates 620B, 620D, 620F, and 620H further comprise a plurality of through-bores, i.e., plurality of through-bores 622B, 622D, 622F, and 622H, respectively. It should be appreciated that, although plates 620A-620H are shown as integral within 30 superior component 602 and inferior component 604, plates 620A-620H could also be discrete plates, fixedly secured to superior component 602 and inferior component 604.

Superior component 602 and inferior component 604 further comprise at least one first aperture 624 arranged to 35 allow fusion between bone fusing material and the adjacent vertebra and a second aperture 626 located on the front face of device 600 and arranged to allow the introduction of bone fusing material into device 600. Second aperture 626 is illustrated as an arched slot as a non-limiting example, 40 however, it should be appreciated that second aperture 626 could be an aperture of any suitable shape, e.g., triangular, circular, rectangular, elliptical, etc., that would allow for the introduction of bone fusing material into device 600. Superior component 602 has a first surface 603 and inferior 45 component 604 has a first surface 605.

FIG. 34 is a perspective view of stand-alone expandable interbody spinal fusion device 600, in an expanded state. It should be appreciated that FIG. 34 is a partial view, i.e., superior component 602 has been removed for clarity. 50 During surgery and after device 600 is implanted in disc space 12, a surgeon can apply torque to expansion mechanisms 606, 608, and 610 via any device that imparts rotational force upon expansion mechanisms 606, 608, and 610 (e.g., a screw driver or impact driver). Expansion mecha- 55 nisms 606, 608 and 610 are preferably the embodiment illustrated in FIGS. 15 and 16, described supra. Furthermore, it should be appreciated that although expansion mechanisms 606, 608, and 610 are depicted within inferior component 604 in FIGS. 33-38, expansion mechanisms 606, 60 608, and 610 could be arranged within superior component 602. The rotational force causes expansion mechanisms 606, 608, and 610 to displace superior component 602 in direction DR1 relative to inferior component 604 giving device **600** an expanded height H₂, greater than H₁ (shown in FIGS. 65 37 and 38). It should be appreciated that expansion mechanisms 606, 608, and 610 can be expanded to any height

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between unexpanded height H₁ and expanded height H₂. Device 600 further comprises post 628. Post 628 is provided to secure locking mechanisms 612 and 616 in position once device 600 is expanded to its final height. Post 628 comprises first section 638, second section 640, third section 642, and fourth section 644. First section 638 has a first end 632, a second end 634, and a flange 636. First end 632 is operatively arranged to engage with any device known in the art that can impart rotational motion onto first section 638, e.g., a drill. Second end 634 is arranged non-rotatably secure to second section 640. Second section 640 includes external helical male threading 646. Third section 642 includes a substantially hollow shaft with cavity 650. Cavity 650 includes internal helical female threading 651 operatively arranged to engage with male threading 646. Fourth section 644 includes cylindrical portion 647 non-rotatably secured to third section 642 and stopping element 648 which is embodied as a substantially rectangular member operatively arranged to abut the surface of plate 620F and prevent movement of post 628 in direction DR3. Second section 640 has a diameter D1. Third section 642 has diameter D2 larger than D1. Cylindrical portion 647 of fourth section 644 has diameter D3 larger than D2, and stopping element 648 has diameter D4 larger than D3. Flange 636 has diameter D4 larger than D3.

Prior to locking, first end 632 of first section 638 is slidingly engaged with through-bore 622A (shown in FIG. 33); second section 640 is loosely seated in the longitudinal space formed between each through-bore of plurality of through-bores 622B of plate 620B; third section 642 is loosely seated in the longitudinal space formed between each through-bore of plurality of through-bores 622F of plate 620F; and cylindrical portion 647 of fourth section 644 is slidingly engaged with square through-bore 622E of plate 620F.

After device 600 has been inserted into disc space 12 and expanded to an appropriate height, a surgeon can apply torque to first end 632 of first section 638. The torque is then transferred to second section 640 having male threading **646**. Second section **640** engages with female threading **651** in cavity 650 of third section 642, pulling post 628 in direction DR3 into the locked position. In the locked position, flange 636 abuts the surface of plate 620A preventing further displacement in direction DR4, and second end 634 of first section 638 is completely seated in one of the through-bores of plurality of through-bores 622B which corresponds to the chosen device height. In this locked position, device 600 is prevented from collapsing in direction DR2. Additionally, in the locked position, cylindrical portion 647 of fourth section 644 is completely seated in one of the through-bores of plurality of through-bores 622F of plate 620F, and stopping element 648 abuts the outer surface of plate 620F, thereby preventing further displacement of third section 642 and fourth section 644 in direction DR3.

Device 600 further comprises post 652 (shown in FIGS. 34, 36, and 38). Post 652 is provided to secure locking mechanisms 614 and 618 in position once device 600 is expanded to its final height. Post 652 further comprises first section 662, second section 644, third section 666, and fourth section 668. First section 662 includes first end 656, second end 658, and flange 660. First end 656 includes a recess operatively arranged to engage with any device known in the art that can impart rotational motion onto first section 662, e.g., a drill. Second end 658 is non-rotatably secured to second section 664. Second section 664 includes external helical male threading 670. Third section 666 includes a substantially hollow shaft with cavity 674. Cavity

674 includes internal helical female threading 675 operatively arranged to engage with male threading 670. Fourth section 668 includes cylindrical portion 671 non-rotatably secured to third section 666 and stopping element 672, which is embodied as a substantially rectangular member 5 operatively arranged to abut the surface of plate 620H and prevent movement of post 652 in direction DR3. Second section 664 has a diameter D1. Third section 666 has diameter D2 larger than D1. Cylindrical portion 671 of fourth section 668 has diameter D3 larger than D2, and 10 stopping element 672 has diameter D4 larger than D3. Flange 660 has diameter D4 larger than D3.

After device 600 has been inserted into disc space 12 and expanded to an appropriate height, a surgeon can apply torque to first end 656 of first section 662. The torque is then 15 transferred to second section 664 having male threading 670. Second section 664 engages with female threading 675 in cavity 674 of third section 666, pulling post 652 in direction DR3 into the locked position. In the locked position, flange 660 abuts the surface of plate 620C preventing 20 further displacement in direction DR4, second end 658 of first section 662 is completely seated in one of the throughbores of plurality of through-bores 622D which corresponds to the chosen device height. In this locked position, device 600 is prevented from collapsing in direction DR2. Addi- 25 tionally, in the locked position, cylindrical portion 671 of fourth section 668 is completely seated in one of the through-bores of plurality of through-bores 622H of plate 620H, and stopping element 672 abuts the outer surface of plate 620F, thereby preventing further displacement of third 30 section 642 and fourth section 644 in direction DR3.

FIG. 39 is a partial front perspective view of a locking mechanism 720 in an unlocked state. Locking mechanism 720 comprises plate 722, plate 724, and fastener 726. Plates 722 and 724 are fixedly secured to superior component 702 35 and inferior component 704 (discussed infra), respectively. Plate 722 includes plurality of catches 730 and plate 724 includes through-bore 732. Through-bore 732 has female threading 734. Plurality of catches 730 is illustrated as a plurality of tapered depressions having a taper back section 40 and a flat ridge similar to a ratchet mechanism, which is arranged to prevent motion in one direction while allowing motion in a second direction. Fastener 726 includes first end 740 and second end 742. Second end 742 has diameter D1 and includes male threading 744 operatively arranged to 45 engage with female threading 734 of through-bore 732. First end 740 of fastener 726 has diameter D2 larger than D1. First end 740 is operatively arranged to engage with any device known in the art that can impart rotational motion onto fastener 726, e.g., a drill. Each catch of plurality of 50 catches 730 has a width greater than or equal to diameter D2.

Before locking, fastener 726 is loosely engaged with female threading 734 of through-bore 732. During surgery, and after device 700 (discussed infra) has been expanded to its final height, a surgeon imparts rotational motion to 55 fastener 726. Male threading 744 of fastener 726 further engages with female threading 734 of through-bore 732 which pulls fastener 726 in direction DR4. When second end 742 of fastener 726 is engaged with one of the catches of plurality of catches 730, device 700 is locked and prevented from collapsing in direction DR2. FIG. 40 is a partial front perspective view of a locking mechanism 720 in a locked state. When device 700 is in the fully collapsed state, plates 722 and 724 nest within recesses 718.

FIG. 41 is a front perspective view of device 700 with 65 locking mechanisms 714 and 716, in an unexpanded state. Device 700 comprises superior component 702, inferior

component 704, and expansion mechanism 710 arranged to displace superior component 702 in a first direction DR1 relative to inferior component 704. Superior component 702 and inferior component 704 further comprise at least one first aperture 706 and at least one second aperture 708, which are arranged to allow fusion between bone fusing material and the adjacent vertebra. Superior component 702 has a first surface 703, and inferior component 704 has a first surface 705. Device 700 further comprises hinge 712 fixedly secured to superior component 702 and inferior component 704 and arranged to rotatably displace the superior component about axis of rotation AR. Locking mechanisms 714 and 716 are preferably locking mechanism 720 described supra. Expansion mechanism 710 is preferably expansion mechanism 176 described supra. It should be noted that since plates 722 and 724 are fixedly secured to superior and inferior components 702 and 704, respectively, recesses 718 are provided within which plates 722 and 724 can nest while device 700 is in a collapsed state. It should further be appreciated that plates 722 and 724 can be hingedly secured to superior component 702 and inferior component 704, respectively. FIG. 42 is a front perspective view of device 700 with locking mechanisms 714 and 716 in an expanded

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FIG. 43 is a partial front perspective view of a locking mechanism 820 in an unlocked state. Locking mechanism 820 comprises plate 822, plate 824, and fastener 826. Plates 822 and 824 are fixedly secured to superior component 802 and inferior component 804 (discussed infra), respectively. Plate 822 includes plurality of catches 830 and plate 824 includes through-bore 832. Through-bore 832 has female threading 834. Plurality of catches 830 are illustrated as a series of cylindrical partial-through-bores. Fastener 826 includes first end 840 and second end 842. Second end 842 has diameter D1 and includes male threading 844 operatively arranged to engage with female threading 834 of through-bore 832. First end 840 of fastener 826 has diameter D2 larger than D1. First end 840 is operatively arranged to engage with any device known in the art that can impart rotational motion onto fastener 826, e.g., a drill. Each catch of plurality of catches 830 has a width greater than or equal to diameter D2.

Before locking, fastener **826** is loosely engaged with female threading **834** of through-bore **832**. During surgery, and after device **800** (discussed infra) has been expanded to its final height, a surgeon imparts rotational motion to fastener **826**. Male threading **834** of fastener **826** further engages with female threading **834** of through-bore **832**, which pulls fastener **826** in direction DR4. When second end **842** of fastener **826** is engaged with one of the catches of plurality of catches **830**, device **800** is locked and prevented from collapsing in direction DR2. FIG. **44** is a partial front perspective view of a locking mechanism **820** in a locked state. When device **800** is in the fully collapsed state, plates **822** and **824** nest within recesses **818**.

FIG. 45 is a front perspective view of device 800 with locking mechanisms 814 and 816, in an unexpanded state. Device 800 comprises superior component 802, inferior component 804, and expansion mechanism 810 arranged to displace superior component 802 in a first direction DR1 relative to inferior component 804. Superior component 802 and inferior component 804 further comprise at least one first aperture 806 and at least one second aperture 808, which are arranged to allow fusion between bone fusing material and the adjacent vertebra. Superior component 802 has a first surface 803 and inferior component 804 has a first surface 805. Device 800 further comprises hinge 812 fixedly

secured to superior component 802 and inferior component 804, and it is arranged to rotatably displace the superior component about axis of rotation AR. Locking mechanisms 814 and 816 are preferably locking mechanism 820 described supra. Expansion mechanism 810 is preferably 5 expansion mechanism 176 described supra. It should be noted that since plates 822 and 824 are fixedly secured to superior and inferior components 802 and 804, respectively, recesses 818 are provided within which plates 822 and 824 can nest while device 800 is in a collapsed state. It should 10 further be appreciated that plates 822 and 824 can be hingedly secured to superior component 802 and inferior component 804, respectively. FIG. 46 is a front perspective view of device 800 with locking mechanisms 814 and 816 in an expanded state.

FIG. 47 is a front perspective view of expandable interbody spinal fusion device 900. FIG. 47 is a front perspective view of stand-alone expandable interbody spinal fusion device 900 in an expanded state. FIG. 48 is a partial exploded view of stand-alone expandable interbody spinal 20 fusion device 900. FIG. 49 is a detail view of stand-alone expandable interbody spinal fusion device 900 taken generally along detail 49 in FIG. 48. FIG. 50A is a front perspective view of stand-alone expandable interbody spinal fusion device 900. FIG. 50B is a side elevational view of 25 stand-alone expandable interbody spinal fusion device 900. FIG. 51 is a side elevational view of stand-alone expandable interbody spinal fusion device 900 in a collapsed state. Expandable interbody spinal fusion device 900 generally comprises superior component 910, inferior component 940, 30 and one or more locking screws 904A-B. The following description should be read in view of FIGS. 47-51.

Superior component 910 comprises surface 912, protrusion 918, protrusion 922, protrusion 926, and hinge portion 930. Surface 912 is operatively arranged to engage a verte- 35 bra. Surface 912 may further comprise one or more ribs 914 and at least one aperture 916. Aperture 916 is arranged to allow bone material injected into cavity 902 to fuse with the adjacent vertebra. Protrusion 918 extends from surface 912 and engages with slot 952 of inferior component 940. 40 Protrusion 918 comprises a plurality of catches 920. Protrusion 922 extends from surface 912 and engages with slot 948 of inferior component 940. Protrusion 922 comprises a plurality of catches 924. Protrusion 926 comprises throughbore 928. Through-bore 928 is designed such that screw 45 906A can pass therethrough and secure superior component 910 to the adjacent vertebra. In the embodiment shown, through-bore 928 is arranged at an angle to surface 912, said angle being greater than 0 degrees and less 90 degrees (see

Inferior component 940 comprises surface 942, slot 948, slot 925, protrusion 956, and hinge portion 960. Surface 942 is operatively arranged to engage a vertebra. Surface 942 may further comprise one or more ribs 944 and at least one aperture 946. Aperture 946 is arranged to allow bone mate- 55 rial injected into cavity 902 to fuse with the adjacent vertebra. Slot 948 is arranged to engage protrusion 922. Slot 948 comprises hole 950 which is operatively arranged to be aligned with one or more of plurality of catches 924. Slot 952 is arranged to engage protrusion 918. Slot 952 com- 60 prises hole 954, which is operatively arranged to be aligned with one or more of plurality of catches 920. Protrusion 956 comprises through-bore 958. Through-bore 958 is designed such that screw 906B can pass therethrough and secure inferior component 940 to the adjacent vertebra. In the 65 embodiment shown, through-bore 958 is arranged at an angle to surface 942, said angle being greater than 0 degrees

and less 90 degrees (see FIG. 51). Inferior component 940 may further comprise one or more ports 964A-B. Ports 964A-B are operatively arranged to be engaged by a tool such that the user (e.g., a surgeon) can hold expandable interbody spinal fusion device 900 in place between adjacent vertebrae (i.e., in place of the removed disc) while expanding superior component 910 with respect to inferior component 940.

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When assembled, superior component 910 is hingedly secured to inferior component 940, and cavity 902 is formed therebetween. As shown, cup-shaped hinge portion 960 is arranged at least partially concentrically around pin-shaped hinge portion 930. In some embodiments, hinge portion 960 is pin-shaped and hinge portion 930 is cup-shaped, with hinge portion 930 concentrically arranged around hinge portion 960. In some embodiments, hinge portions 930 and 960 comprise through-bores through which a pin is passed, to form a normal pin-style hinge between superior component 910 and inferior component 940. Superior component 910 comprises surface 932 and inferior component 940 comprises surface 962. In a collapsed state, as shown in FIG. 51, surface 932 abuts against (or is arranged substantially proximate to) surface 962. In an expanded state, as shown in FIGS. 47-50B, surface 932 is spaced apart from surface 962. To expand expandable interbody spinal fusion device 900, locking screws 904A-B are removed and superior component 910 is hingedly expanded to a desired height. Once expandable interbody spinal fusion device 900 has been expanded to the desired height, locking screws 904A-B are reinserted to lock superior component 910 and inferior component 940. Specifically, locking screw 904A is inserted through the catch of plurality of catches 924 that is aligned with hole 950 and screwed into inferior component 940. As locking screw 904A is tightened in hole 950, a locking portion of locking screw $\bar{904}\mathrm{A}$ engages the aligned catch, thereby locking expandable interbody spinal fusion device 900 at its set height. Similarly, locking screw 904B is inserted through the catch of plurality of catches 920 that is aligned with hole 954 and screwed into inferior component 940. As locking screw 904B is tightened in hole 954, a locking portion of locking screw 904B engages the aligned catch thereby locking expandable interbody spinal fusion device 900 at its set height. Once expandable interbody spinal fusion device 900 is locked at its desired height, screws 906A-B are inserted through through-bores 928 and 958, respectively, securing superior component 910 and inferior component 940 to adjacent vertebrae. Expandable interbody spinal fusion device 900, specifically cavity 902, may then be filled with bone fusion material. In some embodiments, locking screws 904A-B are not arranged to be completely removed from inferior component 940, and comprise retention rings such that they cannot be removed from inferior component 940. In such embodiments, locking screws 904A-B are unscrewed from inferior component 940 until such is prevented by the retention rings, at which point the locking portion of locking screws 904A-B are clear of catches 924 and 920, respectively, and superior component 910 can be expanded/collapsed with respect to inferior component 940

It will be appreciated that various aspects of the disclosure above and other features and functions, or alternatives thereof, may be desirably combined into many other different systems or applications. Various presently unforeseen or unanticipated alternatives, modifications, variations, or improvements therein may be subsequently made by those skilled in the art which are also intended to be encompassed by the following claims.

21 LIST OF REFERENCE NUMERALS 130 Fastener

21		22
LIST OF REFERENCE NUMERALS		130 Fastener
EIGT OF REFERENCE POPULE		132 First end
10 Cainel column		
10 Spinal column		134 Second end
C1-C7 Cervical vertebrae		136 Female threading
T1-T9 Thoracic vertebrae	5	138 First section
L1-L5 Lumbar vertebrae		140 Second section
S Sacrum		142 Third section
C Coccyx		144 Fourth section
D1 First diameter		146 Male threading
D2 Second diameter	10	148 Stopping element
D3 Third diameter		150 Longitudinal space
D4 Fourth diameter		152 Post
DR1 Direction		154 Fastener
DR2 Direction		156 First end
	1.5	
DR3 Direction	15	158 Second end
DR4 Direction		160 Female threading
DL1-L2 Disc		162 First section
DL2-L3 Disc		164 Second section
DL3-L4 Disc		166 Third section
DL4-L5 Disc	20	168 Fourth section
F Facet		170 Male threading
FJ Facet joint		172 Stopping element
H1 Collapsed height		174 Longitudinal space
H2 Expanded height		176 Expansion mechanism
SP Spinous process	25	178 Threaded rod
	23	180 Threaded sleeve
TP Transverse process		
IF Intervertebral foramen		182 Worm drive
A Annulus		184 Worm
AR Axis of rotation		186 Gear
N Nucleus	30	200 Second embodiment
NC Neural canal		202 Superior component
H1 Unexpanded height		203 First surface
H2 Expanded height		204 Inferior component
RD1 Rotational direction 1		205 Second surface
RD2 Rotational direction 2	35	206 First aperture
12 Disc space	33	208 Second Aperture
•		
100 Device		210 Expansion mechanism
102 Superior component		212 Hinge
103 First surface		214 Locking Mechanism
104 Inferior component	40	216 Locking Mechanism
105 Second surface		220 Locking mechanism
106 Expansion mechanism		222 Plate
108 Expansion mechanism		224 Pawl
110 Expansion mechanism		226 Biasing element
112 Locking mechanism	45	228 Post
114 Locking mechanism		230 Fastener
116 Locking mechanism		232 First surface
118 Locking mechanism		234 Second surface
120A Plate		236 Corner
120B Plate	50	238 Hinge
120C Plate	30	240 Through-bore
120D Plate		242 First plurality of teeth
120E Plate		244 Second plurality of teeth
120F Plate		246 Through-bore
120G Plate	55	248 First pawl head
120H Plate		250 Second pawl head
122A Through-bores		252 Hinge
122B Through-bores		254 First protrusion
122C Through-bores		256 Second protrusion
122D Through-bores	60	258 First end
122E Through-bores		260 Second end
122F Through-bores		262 Male threading
122G Through-bores		264 Stopping element
		266 First end
122H Through-bores	65	
124 First aperture	65	268 Second end
126 Second aperture		270 Female threading
128 Post		276 Expansion mechanism

	Threaded rod		504 Inferior component
	Lifting nut		505 Second surface
	Worm drive		506 First aperture
	Worm		508 Second aperture
	Gear	5	510 Expansion mechanism
	Platform		512 Hinge
	Device		514 Locking mechanism
	Superior component		516 Locking mechanism
	First surface		518 Recess
	Inferior component	10	520 Locking mechanism
	Second surface		522 Plate
	First aperture		524 Plate
	Second aperture		526 Fastener
	Expansion mechanism		530 Plurality of through-bores
	Hinge	15	532 Plurality of through-bores
	Locking Mechanism		534 Longitudinal space
	Locking Mechanism		540 First end
	Locking mechanism Plate		542 Second end
	Post	20	544 Male threading
	Fastener	20	600 Device
			602 Superior component
	Corner		603 First surface
	Hinge Plurality of through-bores		604 Inferior component 605 Second surface
	Longitudinal space	25	606 Expansion mechanism
	First end	25	608 Expansion mechanism
	Second end		610 Expansion mechanism
	Male threading		612 Locking mechanism
	Hinge		614 Locking mechanism
	First protrusion	30	616 Locking mechanism
	Second protrusion	30	618 Locking mechanism
	First end		620A Plate
	Second end		620B Plate
	Flange		620 C Plate
	Female threading	35	620D Plate
	Locking mechanism	33	620E Plate
	Plate		620F Plate
	Plate		620G Plate
	Post		620H Plate
	Fastener	40	622A Through-bore
	Plurality of through-bores		622 B Through-bores
	Plurality of through-bores		622C Through-bore
	Longitudinal space		622D Through-bores
	Longitudinal space		622 E Square through-bore
	First end	45	622 F Through-bores
440	Second end		622G Square through-bore
442	Male threading		622H Through-bores
	Shoulder		624 First aperture
446	Stopping element		626 Second aperture
448	First end	50	628 Post
450	Second end		630 Fastener
452	Female threading		632 First end
400	Device		634 Second end
402	Superior component		636 Flange
	First surface	55	638 First section
404	Inferior component		640 Second section
405	Second surface		642 Third section
	First aperture		644 Fourth section
	Second aperture		646 Male threading
	Expansion mechanism	60	647 Cylindrical portion
	Hinge		648 Stopping element
	Locking mechanism		650 Cavity
	Locking mechanism		651 Female threading
	Recess		652 Post
	Device	65	654 Fastener
	Superior component		656 First end
	First surface		658 Second end

660 Flange

662 First section

664 Second section

666 Third section

668 Fourth section

670 Male threading

671 Cylindrical portion

672 Stopping element

674 Cavity

675 Female threading

700 Device

702 Superior component

703 First surface

704 Inferior component

705 Second surface

706 First aperture

708 Second aperture

710 Expansion mechanism

712 Hinge

714 Locking mechanism

716 Locking mechanism

718 Recess

720 Locking mechanism

722 Plate

724 Plate

726 Fastener

730 Plurality of catches

732 Through-bore

734 Female threading

740 First end

742 Second end

744 Male threading

800 Device

802 Superior component

803 First surface

804 Inferior component

805 Second surface

806 First aperture

808 Second aperture

810 Expansion mechanism

812 Hinge

814 Locking mechanism

816 Locking mechanism

818 Recess

820 Locking mechanism

822 Plate

824 Plate

826 Fastener

830 Plurality of catches

832 Through-bore

834 Female threading

840 First end

842 Second end

844 Male threading

900 Device

902 Cavity

904A Locking screw

904B Locking screw

906A Screw

906B Screw

910 Superior component

912 Surface

914 Ribs 916 Aperture

918 Protrusion

920 Catches

922 Protrusion

924 Catches

926 Protrusion

928 Through-bore

930 Hinge portion

932 Surface

940 Inferior component

942 Surface

944 Ribs

946 Aperture

948 Slot

950 Hole

952 Slot

932 SIUL

954 Hole

956 Protrusion

050 Thursday

958 Through-bore

960 Hinge portion

962 Surface

964A Port

₂₀ **964**B Port

What is claimed is:

1. An expandable interbody spinal fusion device, comprising:

an inferior component including at least one hole;

a superior component connected to the inferior component, the superior component including a plurality of catches operatively arranged to align with the at least one hole; and,

a locking screw operatively arranged to extend through the plurality of catches and engage the at least one hole to lock the superior component with respect to the inferior component.

2. The expandable interbody spinal fusion device as so recited in claim 1, wherein the superior component is hingedly connected to the inferior component.

3. The expandable interbody spinal fusion device as recited in claim 1, wherein the superior component comprises a first hinge portion and the inferior component comprises a second hinge portion, the second hinge portion being at least partially concentrically arranged around the first hinge portion.

4. The expandable interbody spinal fusion device as recited in claim 1, wherein the superior component further comprises a first surface including a first aperture.

5. The expandable interbody spinal fusion device as recited in claim 4, wherein the first surface comprises one or more ribs.

6. The expandable interbody spinal fusion device as 50 recited in claim 1, wherein the inferior component further comprises a second surface including a second aperture.

7. The expandable interbody spinal fusion device as recited in claim 6, wherein the second surface comprises one or more ribs.

8. The expandable interbody spinal fusion device as recited in claim 1, wherein the at least one hole is arranged in a slot of the inferior component and the plurality of catches are arranged on a protrusion of the superior component, the protrusion being arranged to engage the slot.

9. The expandable interbody spinal fusion device as recited in claim 1, wherein the inferior component further comprises a first through-bore and the superior component further comprises a second through-bore, the first and second through-bore operatively arranged to engage screws.

10. The expandable interbody spinal fusion device as recited in claim 1, wherein the superior component and the inferior component form a cavity therebetween.

- 11. The expandable interbody spinal fusion device as recited in claim 1, wherein one of the inferior component and superior component comprises one or more ports.
- 12. The expandable interbody spinal fusion device as recited in claim 1, further comprising an expansion mechanism operatively arranged to displace the superior component in a first direction relative to the inferior component.
- 13. An expandable interbody spinal fusion device, comprising:
 - an inferior component including a first surface and at least one hole:
 - a superior component hingedly connected to the inferior component, the superior component including a second surface and a plurality of catches operatively arranged 15 to align with the at least one hole;
 - a cavity formed between the inferior component and the superior component; and,
 - a locking screw operatively arranged to engage the plurality of catches and the at least one hole to lock the ²⁰ superior component with respect to the inferior component.
- 14. The expandable interbody spinal fusion device as recited in claim 13, wherein the superior component comprises a first hinge portion and the inferior component comprises a second hinge portion, the second hinge portion being at least partially concentrically arranged around the first hinge portion.

- 15. The expandable interbody spinal fusion device as recited in claim 13, wherein the first surface comprises a first aperture.
- 16. The expandable interbody spinal fusion device as recited in claim 13, wherein the second surface comprises a second aperture.
- 17. The expandable interbody spinal fusion device as recited in claim 13, wherein the at least one hole is arranged in a slot of the inferior component and the plurality of catches are arranged on a protrusion of the superior component, the protrusion being arranged to engage the slot.
- 18. The expandable interbody spinal fusion device as recited in claim 13, wherein:
 - in a collapsed state, a third surface of the inferior component abuts against a fourth surface of the superior component; and,
 - in an expanded state, the fourth surface is spaced apart from the third surface.
- 19. The expandable interbody spinal fusion device as recited in claim 13, wherein the inferior component further comprises a first through-bore and the superior component further comprises a second through-bore, the first and second through-bore operatively arranged to engage screws to secure the expandable interbody spinal fusion device to one or more vertebrae.
- 20. The expandable interbody spinal fusion device as recited in claim 13, wherein one of the inferior component and superior component comprises one or more ports.

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